

Tuning degradation through molecular structure/ Controlled Release Devices

Last time: factors controlling polymer degradation and erosion
theory of polymer erosion

Today: degradable solid polymer molecular design
fundamental concepts of controlled release devices and applications
controlled release devices based on degradable polymers

Reading:

- W.M. Saltzman and W.L. Olbricht, 'Building drug delivery into tissue engineering, Nat. Rev. Drug Disc. 1, 177-186 (2002)
- W.M. Saltzman 'Drug administration and effectiveness,' from Drug Delivery: Engineering Principles for Drug Therapy, (2001)

Announcements:

Last time

Bulk vs. surface erosion: how do we predict it?

Bulk erosion

Surface erosion

Figures removed for copyright reasons.
Please see:

Fig. 8(b) in Lu, L., C. A. Garcia, and A. G. Mikos.
"In Vitro Degradation of Thin Poly(DL-lactic-co-glycolic acid) Films." *J Bio Med Mater Res* 46 (1999): 236-44.

Images of Surface Erosion removed due to copyright restrictions.

Fig. 6(d) in Agrawal, C. M., and K. A. Athanasiou.
"Technique to Control pH in Vicinity of Biodegrading PLA-PGA Implants." *J Biomed Mater Res* 38 (1997): 105-14.

Göpferich theory of polymer erosion

- If polymer is initially water-insoluble, and hydrolysis is the only mechanism of degradation, then two *rates* dominate erosion behavior:

Rate of water diffusion into polymer matrix

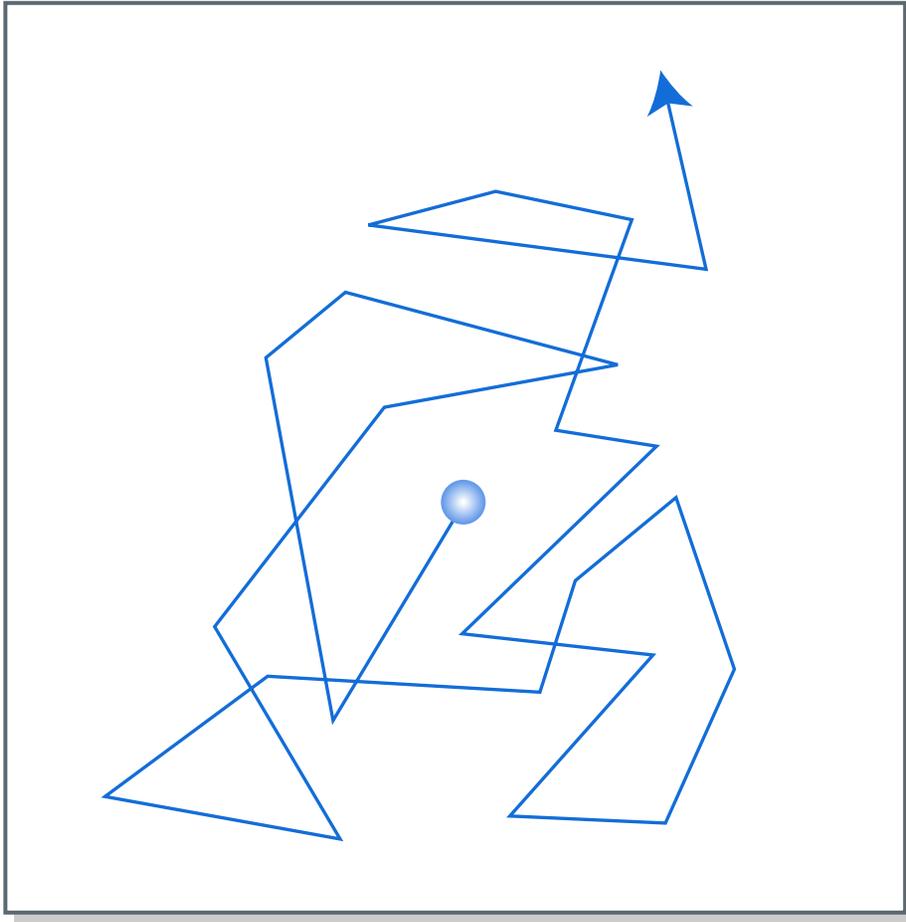
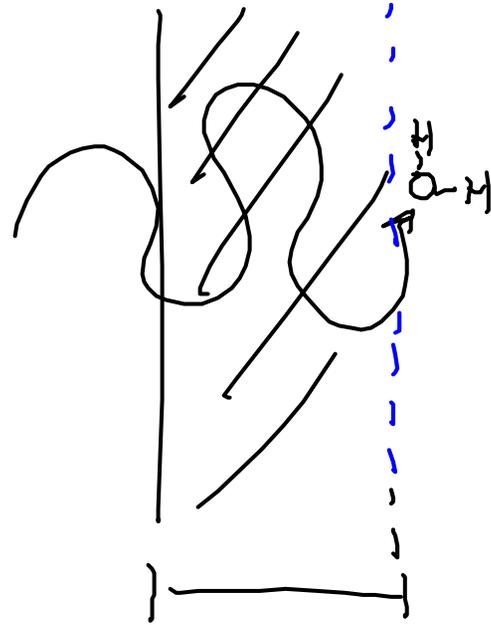
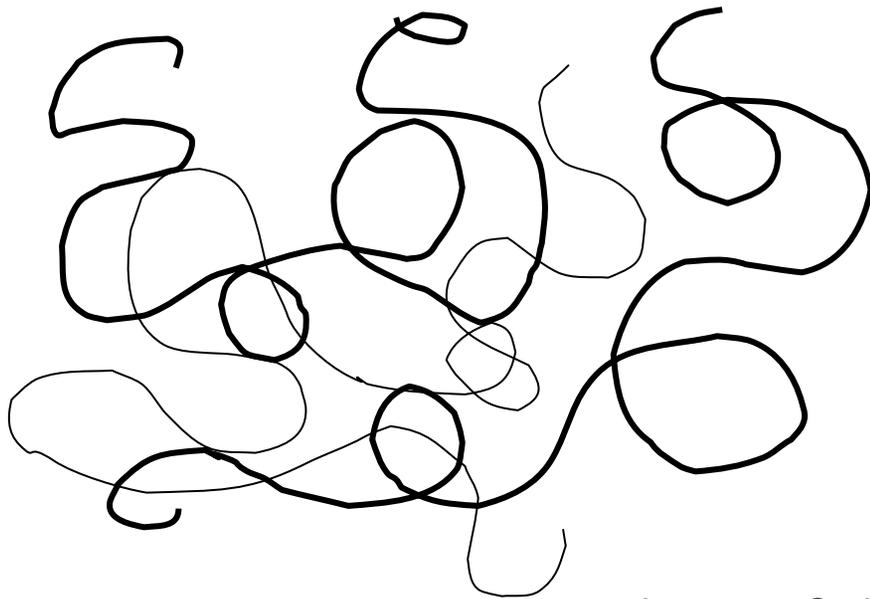


Figure by MIT OCW.



After Atkins, P. *The Elements of Physical Chemistry*. New York, NY: W. H. Freeman, 1997.

Rate of chain cleavage



Rate of chain cleavage

$$p(t) = ke^{-kt}$$

Mean lifetime of one bond:

...this is the mean time I need to wait to observe one bond I am watching be broken.

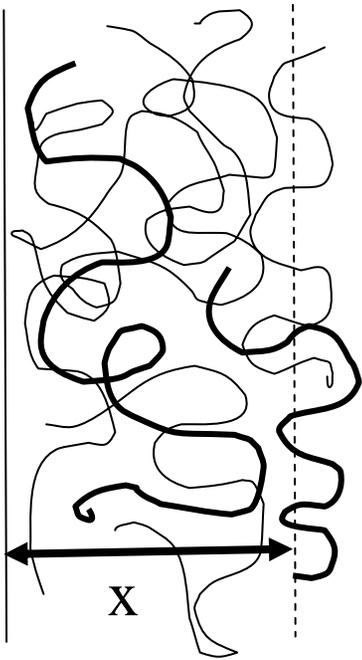
Rate of chain cleavage

Mean lifetime of n bonds:



Rate of chain cleavage

Mean lifetime of n bonds:



How many bonds in a depth x ?

Comparison of water diffusion rate to bond lysis rate allows the qualitative mechanism to be predicted:

$$\varepsilon = \text{erosion number} \equiv \frac{t_{\text{DIFF}}}{t_c(n)}$$

$$\varepsilon \gg 1$$

$\varepsilon \sim 1$ change in
erosion mechanism

$$\varepsilon \ll 1$$

Erosion parameters of degradable polymers

Chemical Structure	Polymer	λ (s ⁻¹)	ϵ^a	$L_{critical}^b$
$\left[\text{R}-\overset{\text{O}}{\parallel}{\text{C}}-\text{O}-\overset{\text{O}}{\parallel}{\text{C}} \right]$	Poly(anhydrides)	1.9×10^{-3} Ref. [30]	11,515	75 μm
$\left[\text{O}-\overset{\text{R}}{\underset{\text{R}}{\text{C}}}-\text{O}-\text{R} \right]$	Poly(ketal)	6.4×10^{-5} Ref. [30]	387	0.4 mm
$\left[\text{O}-\overset{\text{OR}}{\underset{\text{R}}{\text{C}}}-\text{O}-\text{R} \right]$	Poly(ortho esters)	4.8×10^{-5} Ref. [30]	291	0.6 mm
$\left[\text{O}-\overset{\text{H}}{\underset{\text{R}}{\text{C}}}-\text{O}-\text{R} \right]$	Poly(acetal)	2.7×10^{-8} Ref. [30]	0.16	2.4 cm
$\left[\text{O}-(\text{CH}_2)_5-\overset{\text{O}}{\parallel}{\text{C}} \right]$	Poly(ϵ -caprolactone)	9.7×10^{-8} Ref. [31]	0.1	1.3 cm
$\left[\text{O}-\overset{\text{H}}{\underset{\text{CH}_3}{\text{C}}}-\overset{\text{O}}{\parallel}{\text{C}} \right]$	Poly(α -hydroxy-esters)	6.6×10^{-9} Ref. [30]	4.0×10^{-2}	7.4 cm
$\left[\text{N}-\overset{\text{H}}{\underset{\text{R}}{\text{C}}}-\overset{\text{O}}{\parallel}{\text{C}} \right]$	Poly(amides)	2.6×10^{-13} Ref. [30]	1.5×10^{-6}	13.4 m

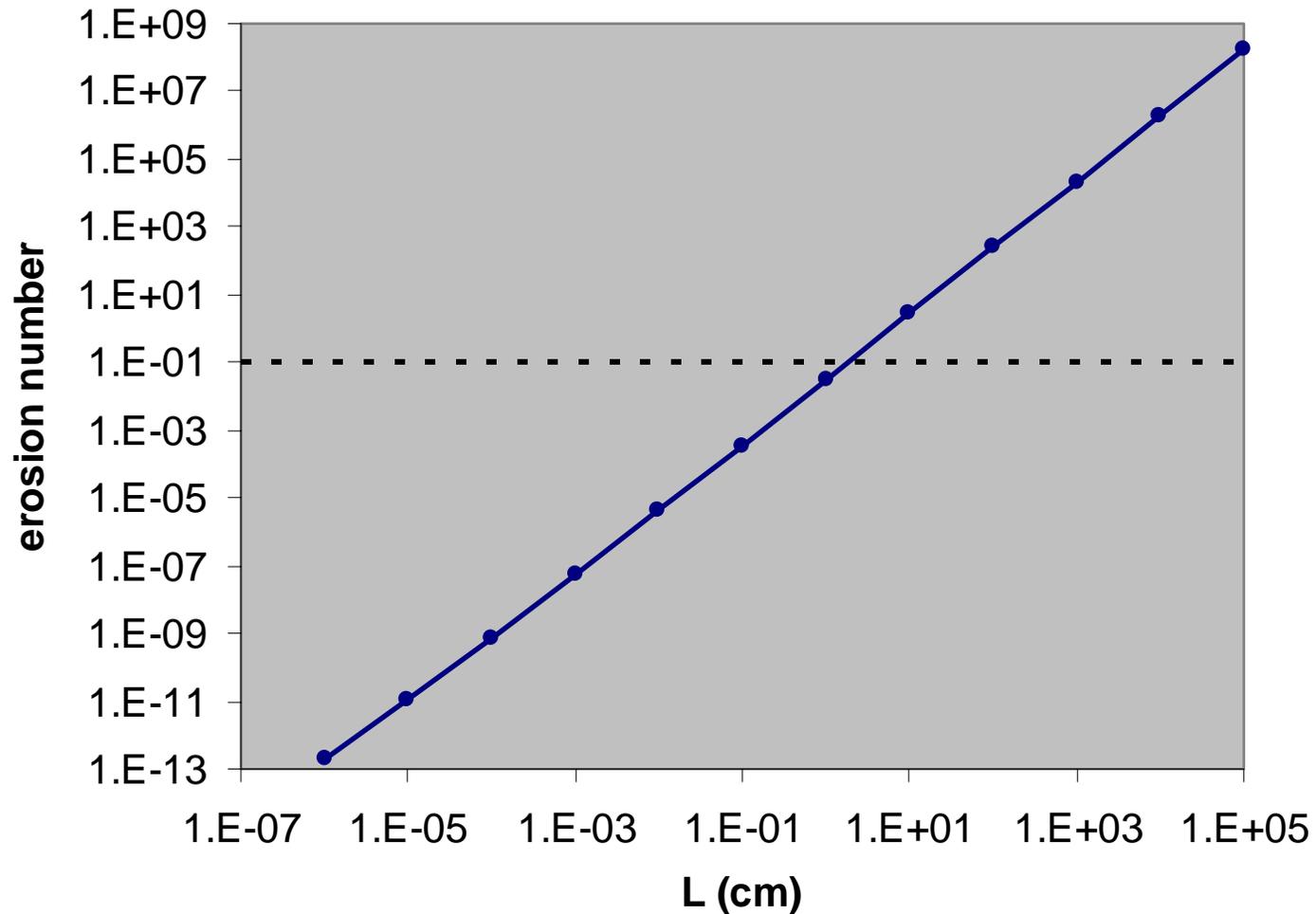
^aFor a 1cm thick device, $D = 10^{-8}\text{cm}^2\text{s}^{-1}$ (estimated from Ref. [32]) and in $\left[\sqrt[3]{\overline{M}_n/N_A(N-1)\rho} \right] = -16.5$.

^b $D = 10^{-8}\text{cm}^2\text{s}^{-1}$ (estimated from Ref. [32]) and in $\left[\sqrt[3]{\overline{M}_n/N_A(N-1)\rho} \right] = -16.5$.

Estimated values of ϵ and $L_{critical}$ for selected degradable polymers

Figure by MIT OCW.

Dependence of erosion number on device dimensions



Testing the theory: experimental switch of a bulk-eroding polymer to a surface-eroding mechanism

PLA and PLGA degradation at pH 7.4: (bulk erosion)

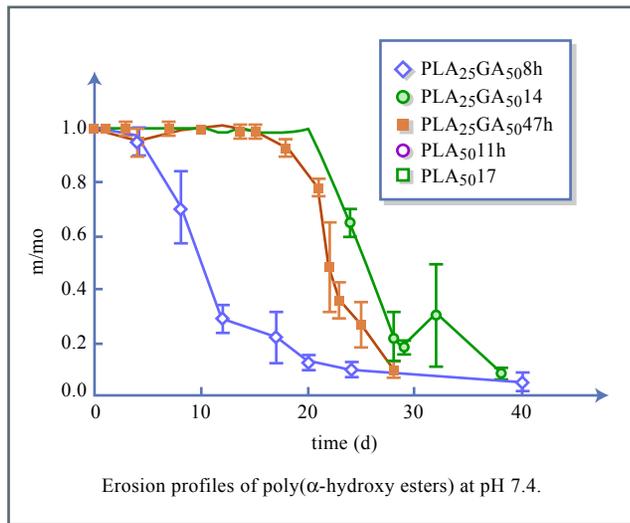


Figure by MIT OCW.

PLA and PLGA degradation at pH 12: (surface erosion)

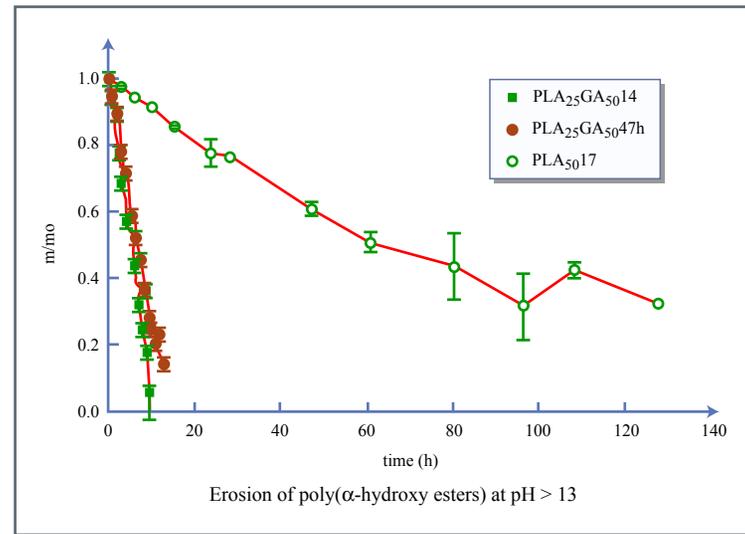


Figure by MIT OCW.

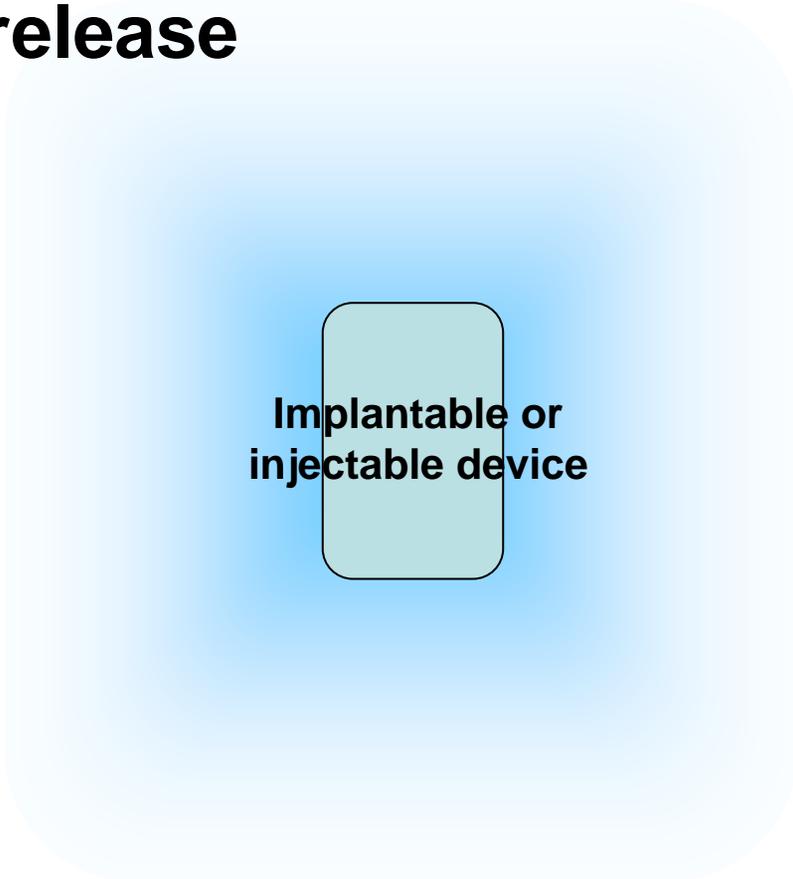
(SEM shown earlier confirms surface erosion mechanism)

Control over polymer degradation by molecular architecture

Controlling molecular architecture: self-assembly

Concepts in controlled release

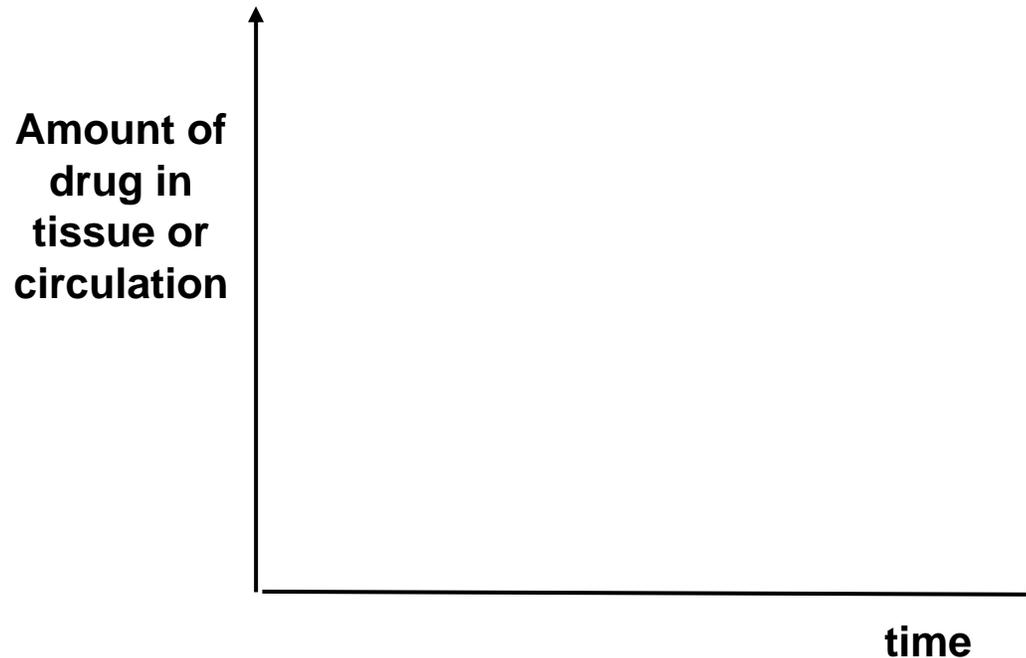
Application of degradable solid polymers to controlled release



Implantable or
injectable device

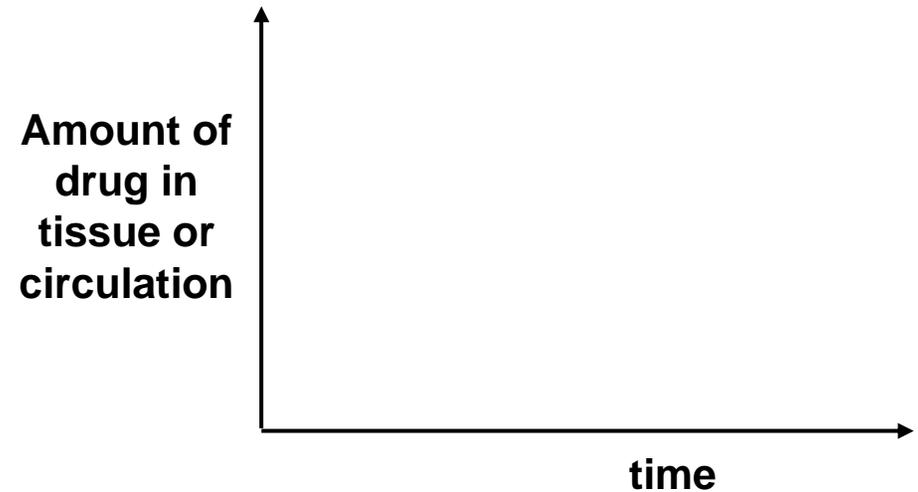
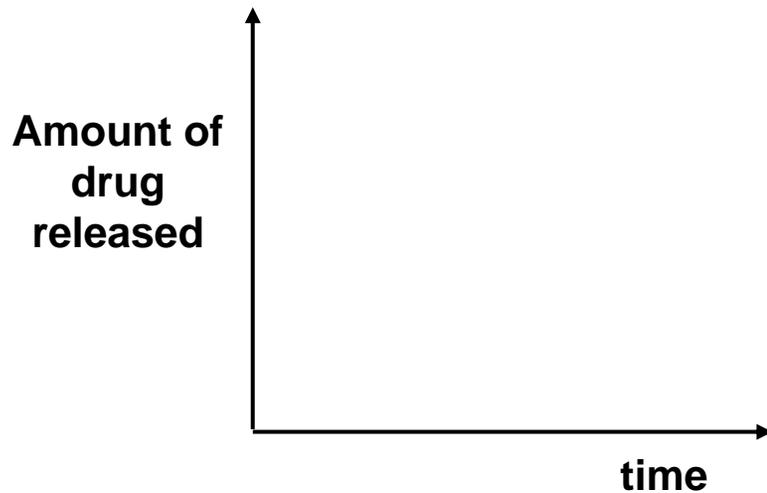
Therapeutic index: tailoring materials to provide release kinetics matching the 'therapeutic window'

Bolus drug injection:



Therapeutic index: tailoring materials to provide release kinetics matching the 'therapeutic window'

Objective of controlled release:

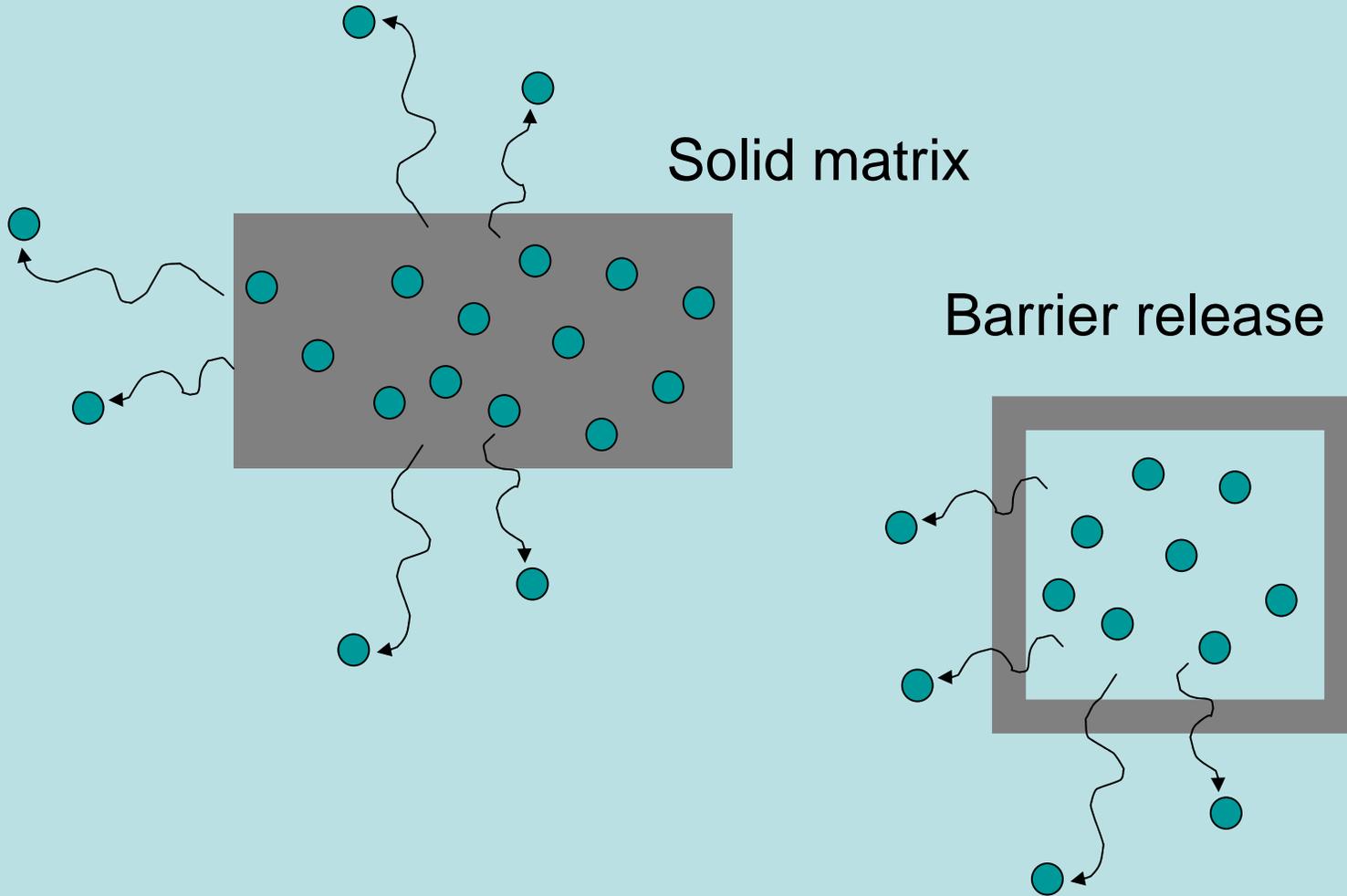


Example applications of controlled release

Application	Examples	Active concentration of cargo
Provide missing soluble factors promoting cell differentiation, growth, survival, or other functions	Replace deficient human growth hormone in children	1-10 pM; Hormones 5-10 nM
Sustained or modulated delivery of a therapeutic drug	Release of anti-cancer drugs at site of tumors to induce cancer cell apoptosis, ocular drugs for treatment of glaucoma, contraceptive drugs, antimalarial drugs	varies
Create gradients of a molecule <i>in situ</i>	Chemoattraction of immune cells to antigen depot for vaccines ¹	1-50 pM
One time procedure (e.g. injection) with multiple dose delivery	Pulsatile release of antigen for vaccines	10-100 µg antigen
Gene therapy	Correction of cystic fibrosis gene defect, correction of adenosine deaminase deficiency (ADA-SCID) in lymphocytes, replace defective gene in Duchenne muscular dystrophy, cancer immunotherapy ²	1-20 µg DNA

Delivery site
Oral (delivery via digestive tract)
Sublingual (under tongue)
Rectal
Parenteral <ul style="list-style-type: none">• intramuscular• peritoneal (gut)• subcutaneous (under skin)
Ocular

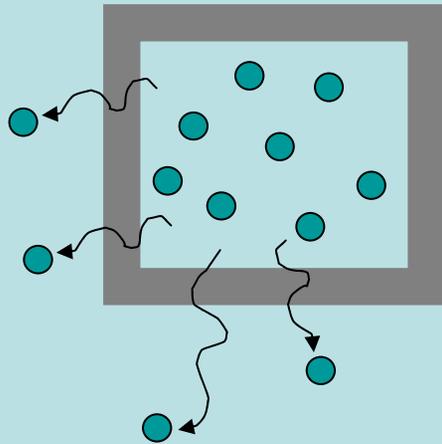
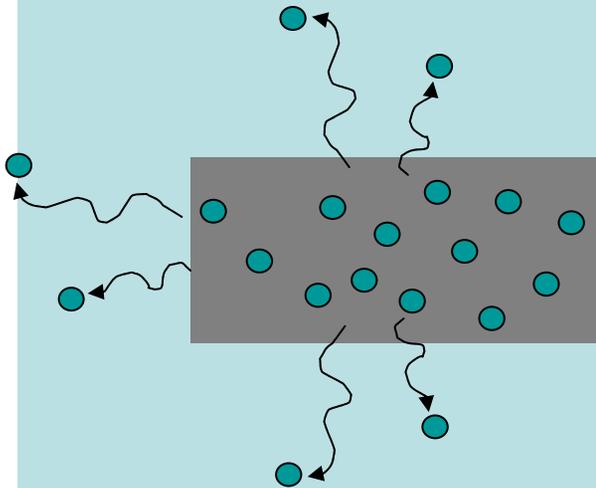
Drug diffusion-controlled release



Drug diffusion-controlled release

Advantage:

Disadvantages:



Further Reading

1. Kumamoto, T. et al. Induction of tumor-specific protective immunity by in situ Langerhans cell vaccine. *Nat Biotechnol* **20**, 64-9 (2002).
2. Dash, P. R. & Seymour, L. W. in *Biomedical Polymers and Polymer Therapeutics* (eds. Chiellini, E., Sunamoto, J., Migliaresi, C., Ottenbrite, R. M. & Cohn, D.) 341-370 (Kluwer, New York, 2001).
3. Baldwin, S. P. & Saltzman, W. M. Materials for protein delivery in tissue engineering. *Adv Drug Deliv Rev* **33**, 71-86 (1998).
4. Okada, H. et al. Drug delivery using biodegradable microspheres. *J. Contr. Rel.* **121**, 121-129 (1994).
5. Santini Jr, J. T., Richards, A. C., Scheidt, R., Cima, M. J. & Langer, R. Microchips as Controlled Drug-Delivery Devices. *Angew Chem Int Ed Engl* **39**, 2396-2407 (2000).
6. Garcia, J. T., Dorta, M. J., Munguia, O., Llabres, M. & Farina, J. B. Biodegradable laminar implants for sustained release of recombinant human growth hormone. *Biomaterials* **23**, 4759-4764 (2002).
7. Jiang, G., Woo, B. H., Kang, F., Singh, J. & DeLuca, P. P. Assessment of protein release kinetics, stability and protein polymer interaction of lysozyme encapsulated poly(D,L-lactide-co-glycolide) microspheres. *J Control Release* **79**, 137-45 (2002).
8. Edlund, U. & Albertsson, A.-C. Degradable polymer microspheres for controlled drug delivery. *Advances in Polymer Science* **157**, 67-112 (2002).
9. Siepmann, J. & Gopferich, A. Mathematical modeling of bioerodible, polymeric drug delivery systems. *Adv Drug Deliv Rev* **48**, 229-47 (2001).
10. Charlier, A., Leclerc, B. & Couarraze, G. Release of mifepristone from biodegradable matrices: experimental and theoretical evaluations. *Int J Pharm* **200**, 115-20 (2000).
11. Fan, L. T. & Singh, S. K. *Controlled Release: A Quantitative Treatment* (eds. Cantow, H.-J. et al.) (Springer-Verlag, New York, 1989).