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Lecture: “Cytoskeleton dynamics simulation of the red blood cell” by Ju Li.  
Given August 17, 2006 during the GEM4 session at MIT in Cambridge, MA.

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# **Cytoskeleton dynamics simulation of the red blood cell**

Ju Li

Collaborators: Subra Suresh, Ming Dao, George Lykotrafitis,  
Chwee-Teck Lim

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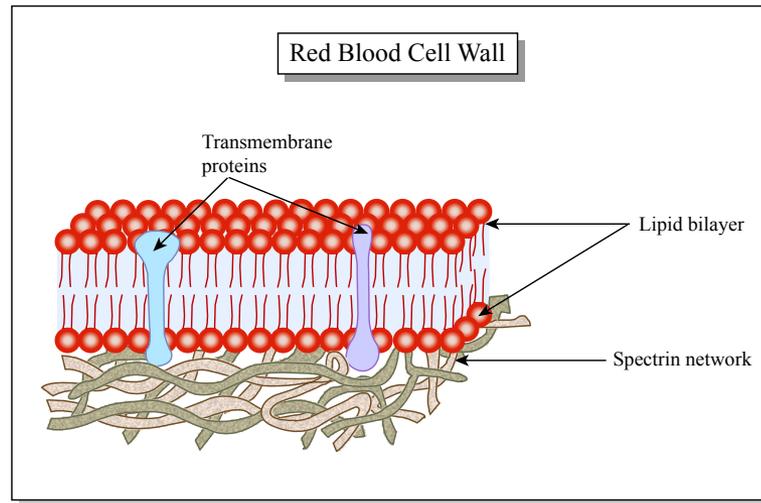
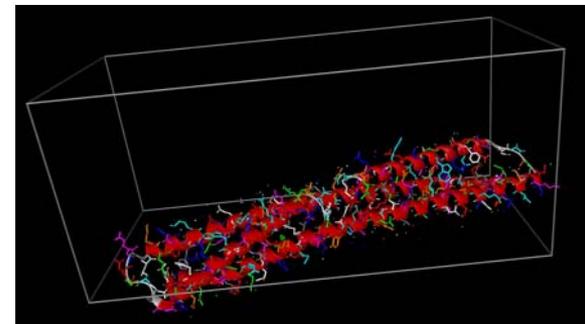
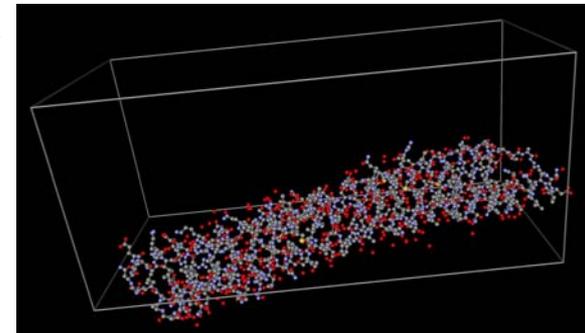


Figure by MIT OCW.

One spectrin tetramer has 39 segments,  
 contour length  $\sim 200$  nm.  
 Room-temperature length  $\sim 80$  nm  
 due to thermal fluctuations.

← one segment  $\sim 5$  nm →

Image removed due to copyright restrictions.



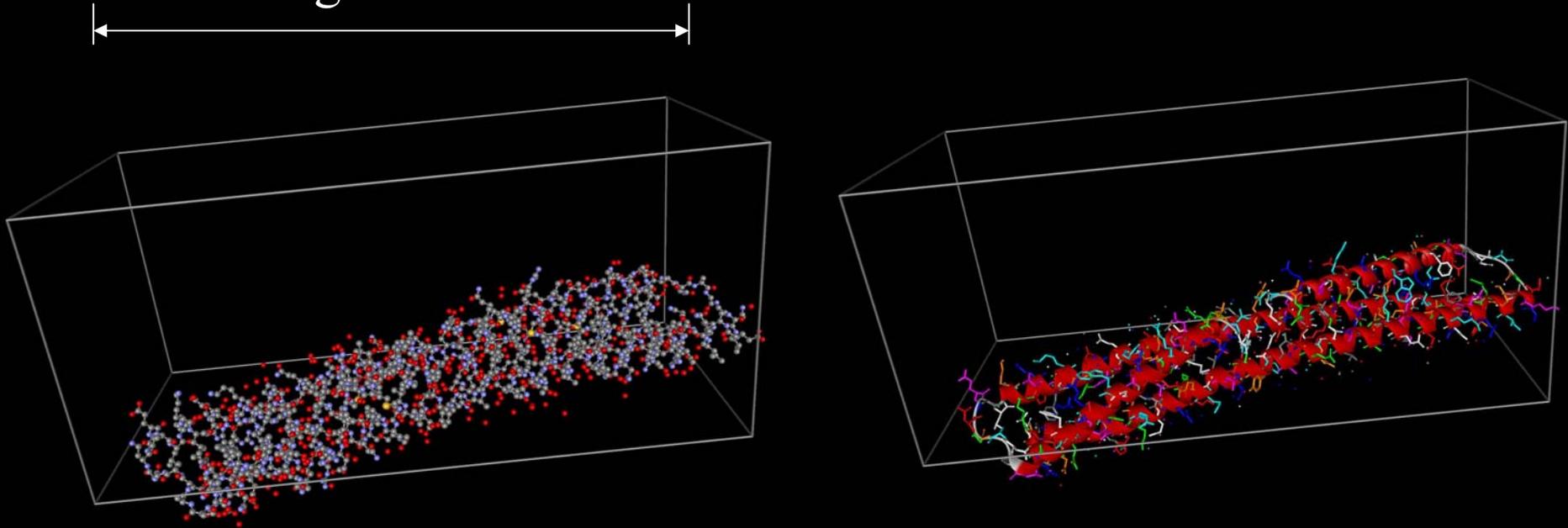
Images removed due to copyright restrictions.  
 See Fig. 2 in Takeuchi, et al. "Structure of the Erythrocyte  
 Membrane Skeleton as Observed by Atomic Force Microscopy."  
*Biophys J* 74 (1998): 2171-2183.

Image removed due to copyright restrictions.

See movies in Dao, M., C. T. Lim, and S. Suresh. "Mechanics of The Human Red Blood Cell Deformed by Optical Tweezers." *J Mech Phys Solids* 51 (2003): 2259-2280.

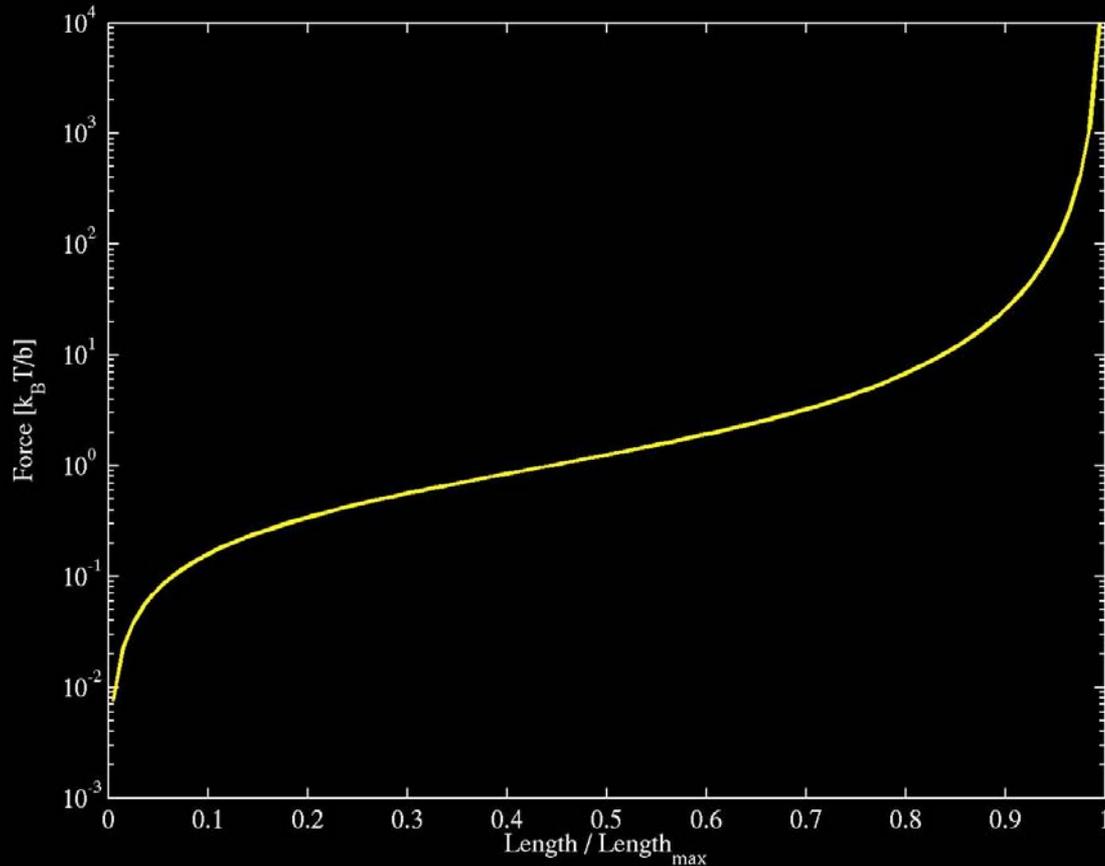
# Spectrin Elasticity

one segment  $\sim 5$  nm



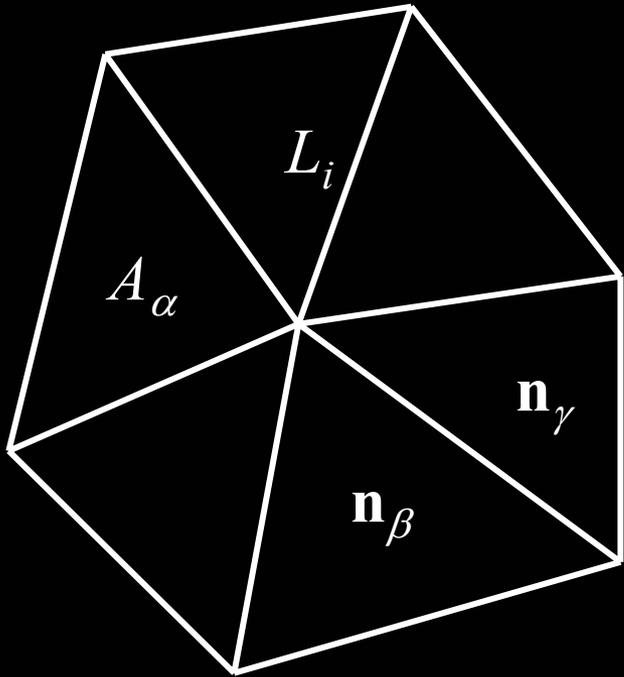
One spectrin tetramer has  $\sim 40$  segments, contour length  $\sim 200$  nm.  
Room-temperature length  $\sim 80$  nm due to thermal fluctuations.

# Worm-like Chain Coarse-Grained Free Energy



$$V_{\text{WLC}}(L) = \frac{k_{\text{B}}TL_{\text{max}}}{4b} \cdot \frac{3x^2 - 2x^3}{1-x}, \quad x \equiv \frac{L}{L_{\text{max}}}$$

# Spectrin-Net Level, Whole Red Blood Cell model (Discher, Boal, Boey, 1998)

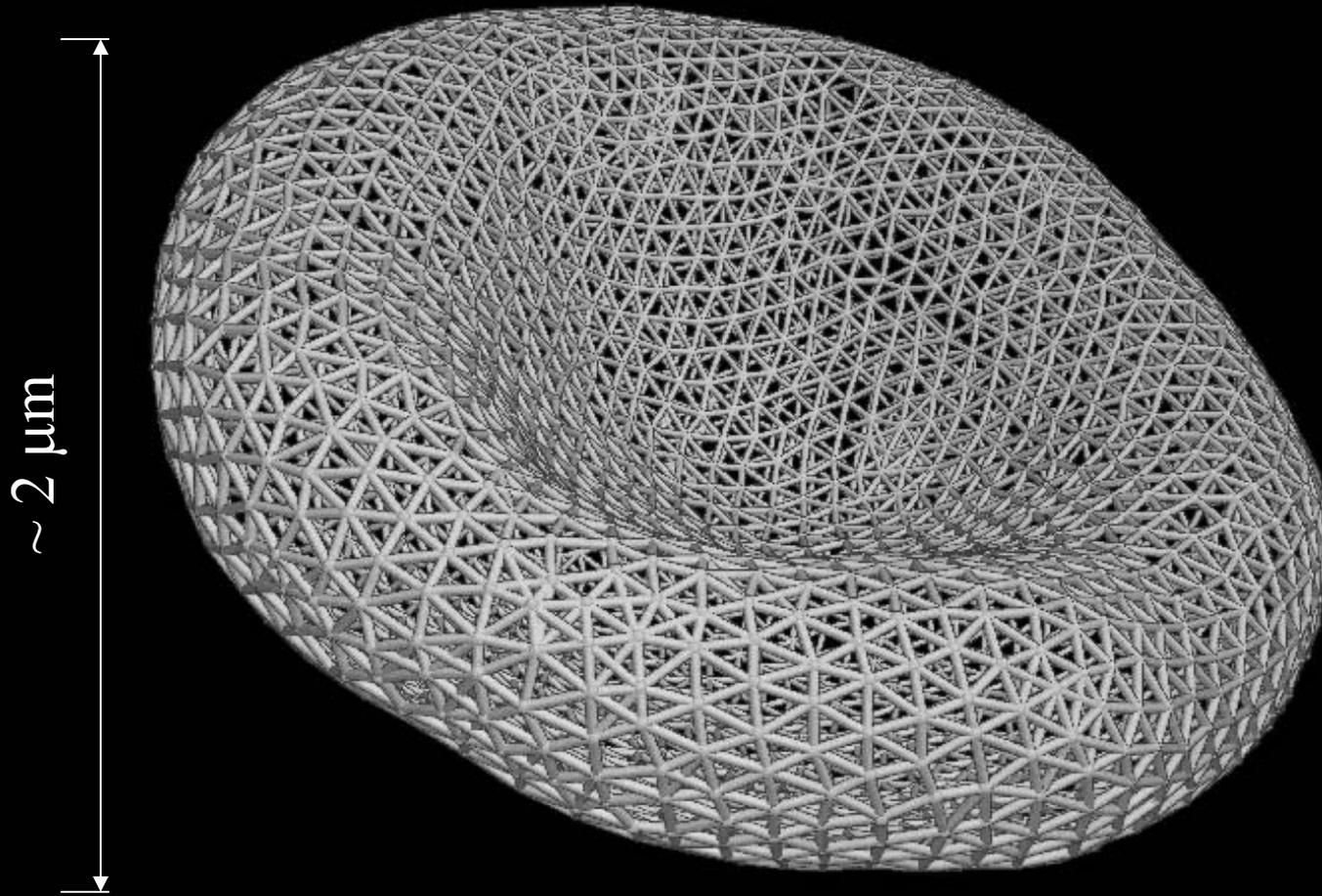


$$V_{\text{total}} = \sum_{i \in \text{spectrin link}} V_{\text{WLC}}(L_i) + \sum_{\alpha \in \text{triangle}} \frac{C}{A_\alpha} + \sum_{\beta, \gamma \in \text{triangle}} K_{\text{bend}} (1 - \mathbf{n}_\beta \cdot \mathbf{n}_\gamma)$$

+ total volume constraint + total area constraint

# Small Cell Simulation

(“volume quench” to get discocyte shape)



2562 vertices

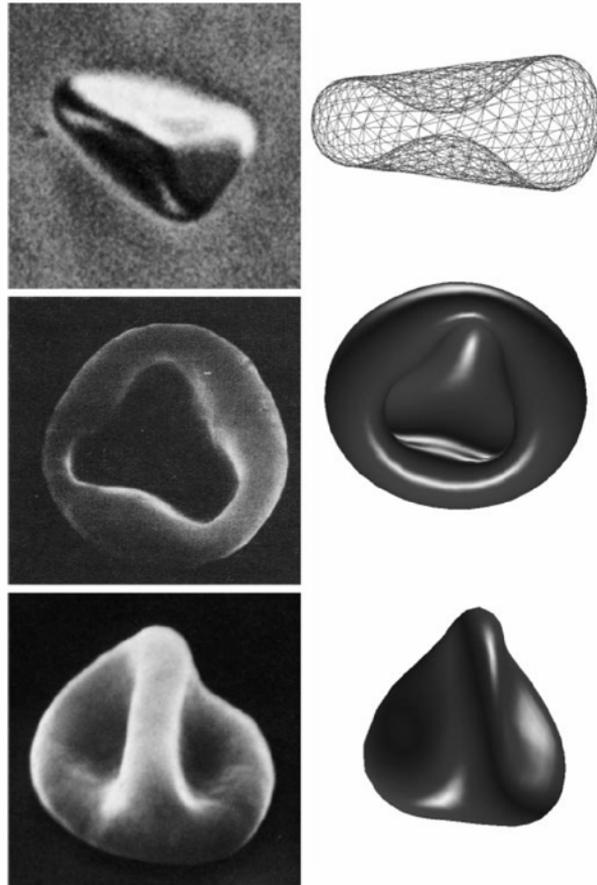
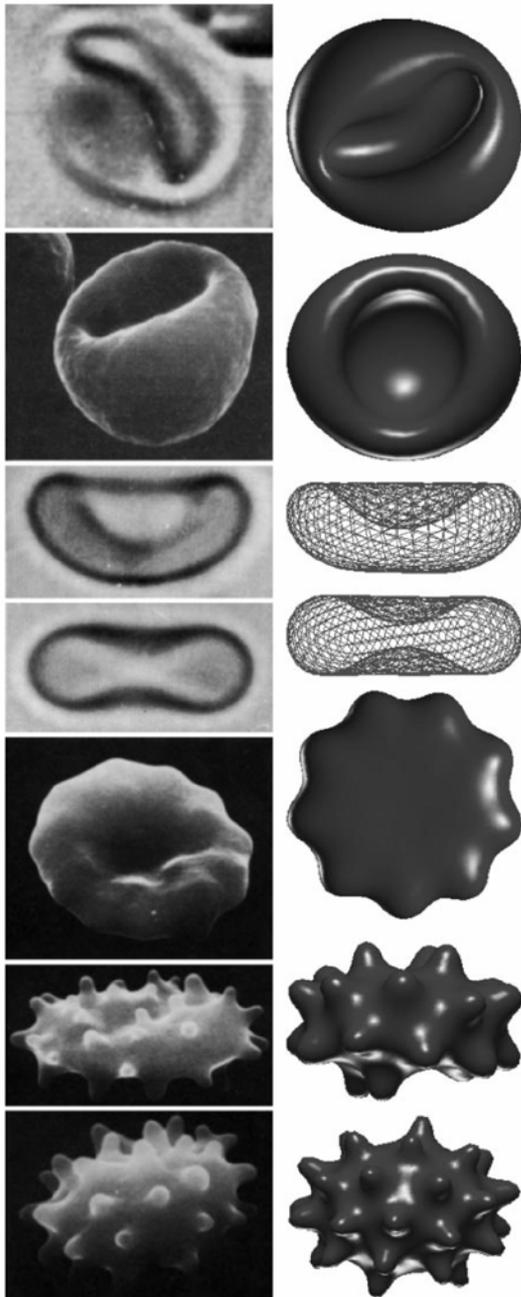


Fig. 2. A sample of observed non-main-sequence shapes, including (top to bottom) nonaxisymmetric discocyte, stomatocyte with triangular mouth, and knizocyte. (Left) Laboratory images reproduced with permission from refs. 27 (Copyright 1981, Biophysical Society), 32 (Copyright 1980, Academic Press), and 2 (Copyright 1973, Springer). (Right) Minimum-energy shapes calculated from our model with values of  $v_0$  and  $\Delta a_0$  of 0.989 and 0.215%, 0.950 and -0.858%, and 1.000 and 1.144% (from top to bottom) with all other parameters remaining fixed.

required to make them conform. The shape-free-energy functional that incorporates these two effects is

$$F_{ADE}[S] = \frac{\kappa_b}{2} \oint_S dA (2H - C_0)^2 + \frac{\bar{\kappa}}{2AD^2} \pi (\Delta A - \Delta A_0)^2, \quad [1]$$

where  $D$  is the membrane thickness,  $A$  is the membrane area,  $\kappa_b$

Lim, Wortis,  
Mukhopadhyay,  
*PNAS* **99** (2002)  
16766

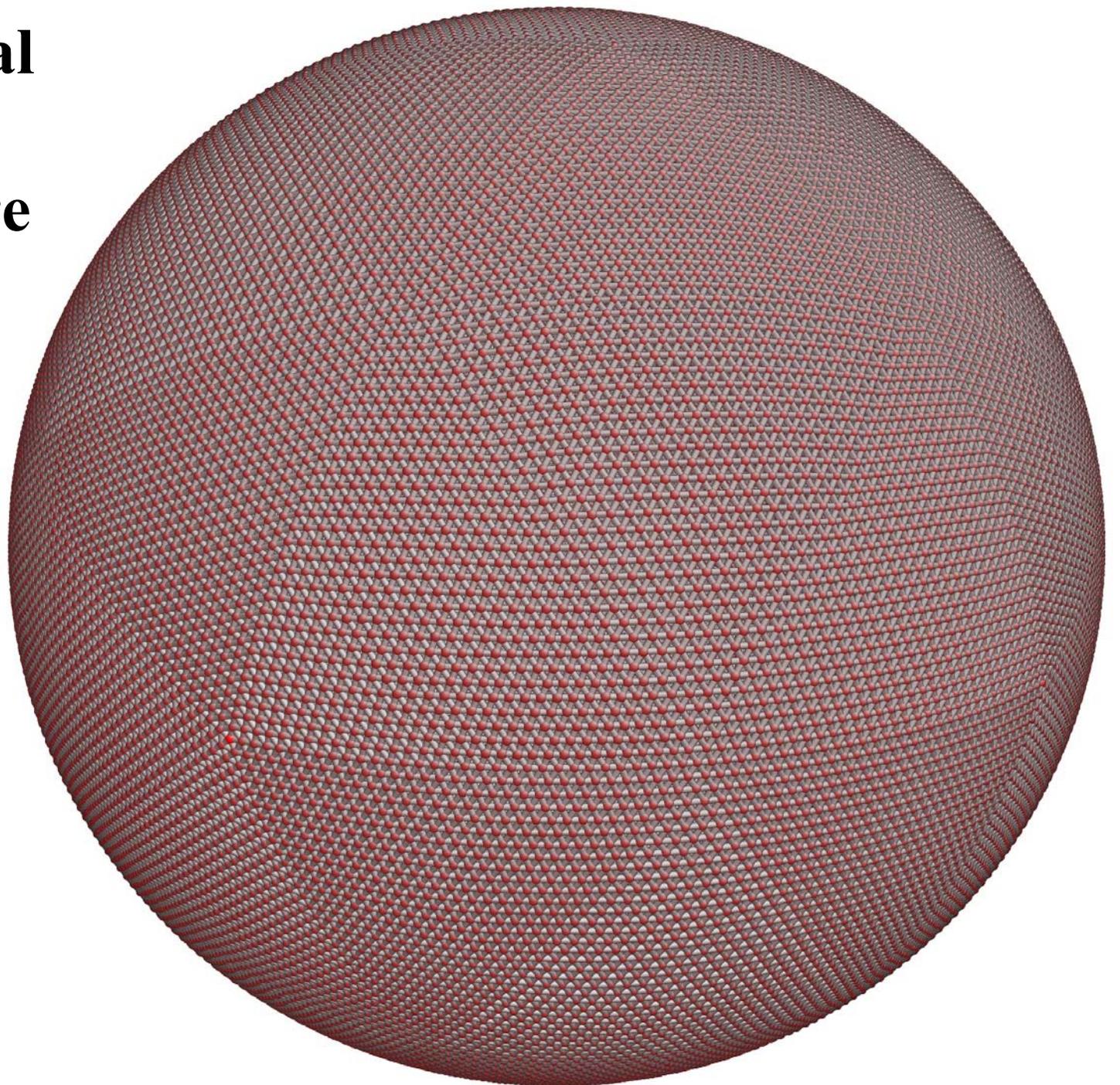
Stomatocyte -  
discocyte -  
echinocyte  
Sequence

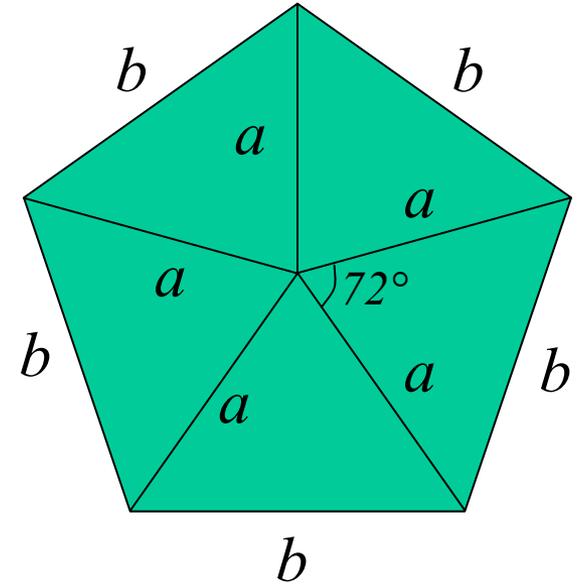
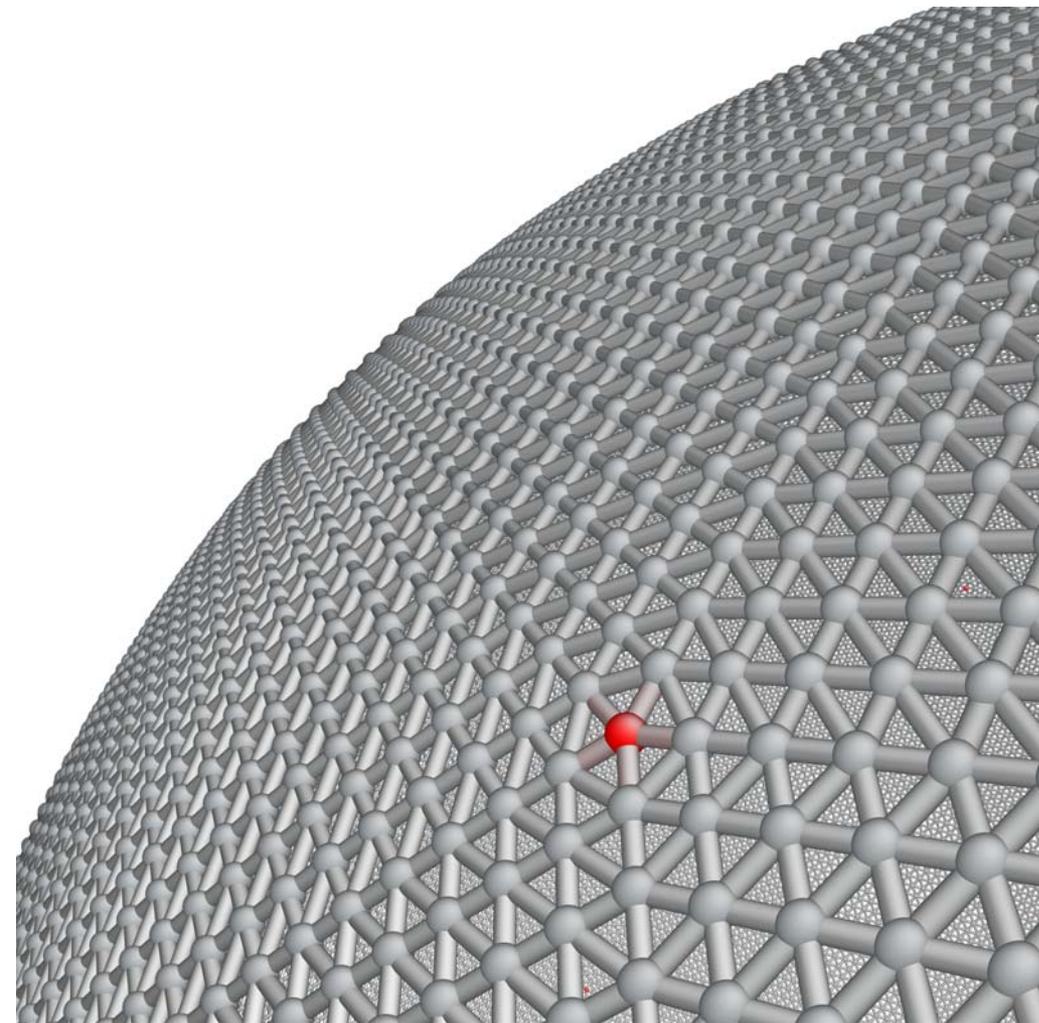
spontaneous  
curvature  
parameter

Courtesy of National Academy of Sciences, U. S. A. Used with permission.

Source: Lim, Gerald, Michael Wortis, and Ranjan Mukhopadhyay. "Stomatocyte–discocyte–echinocyte Sequence of the Human Red Blood Cell: Evidence for the Bilayer– Couple Hypothesis from Membrane Mechanics." *PNAS* 99 (2002): 16766-16769. Copyright 2002 National Academy of Sciences, U.S.A.

# Icosahedral network on a sphere

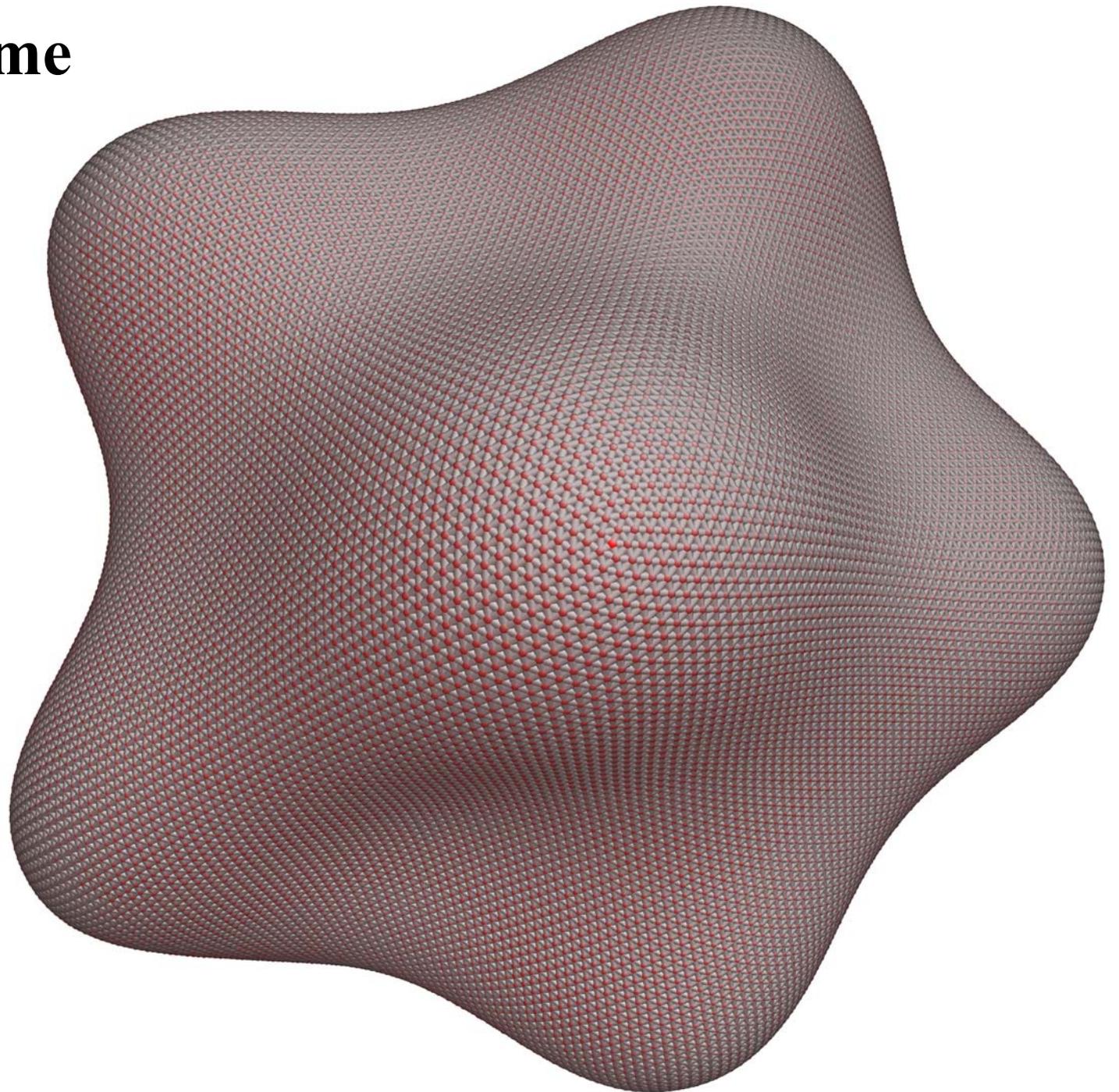




## Geometrically Necessary Disinclinations

If each carries disinclination charge  $60^\circ$ , need 12

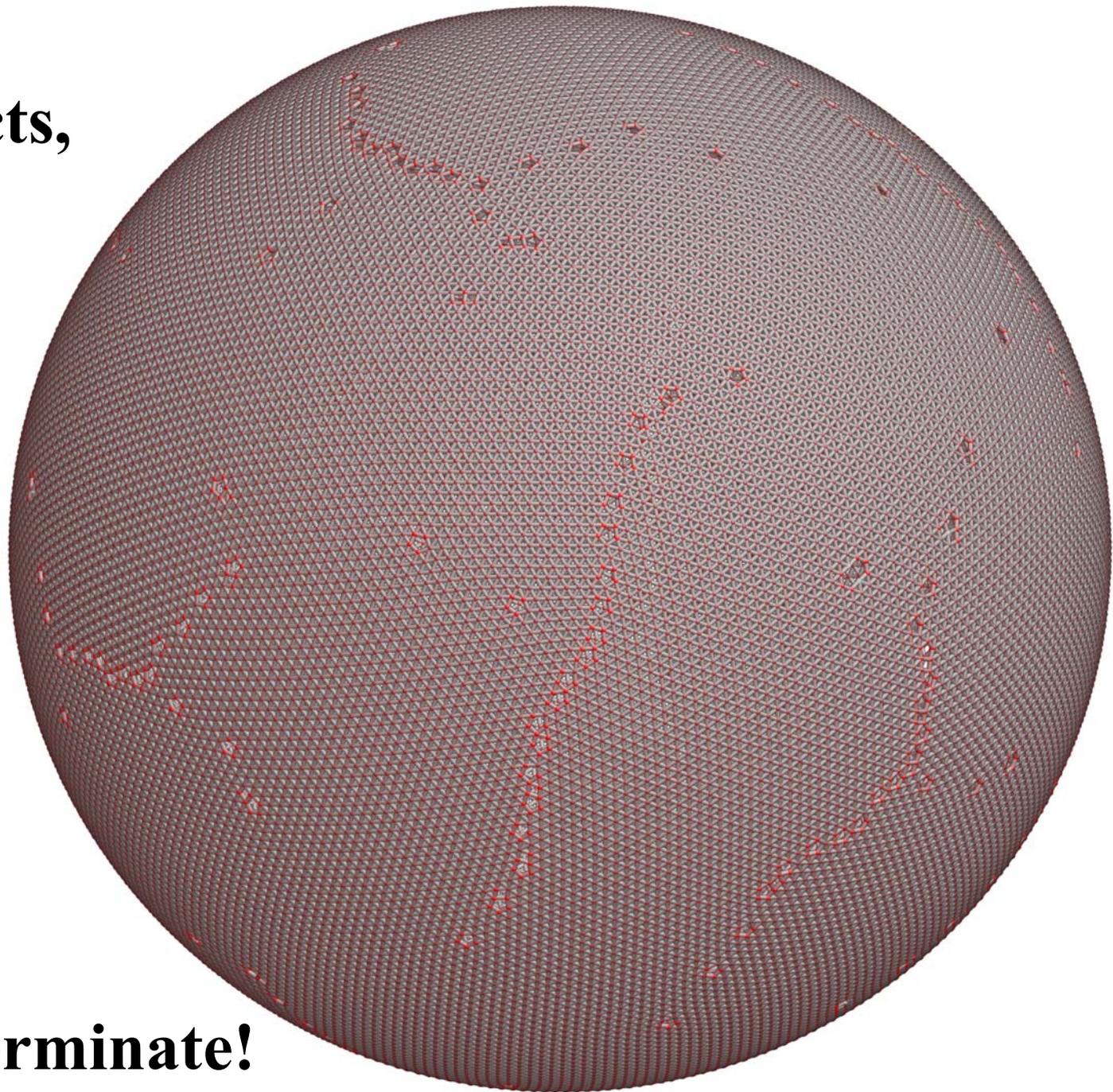
**100% volume**



**60% volume**



**To rid of the  
shape artifacts,  
melt and  
quench the  
network**



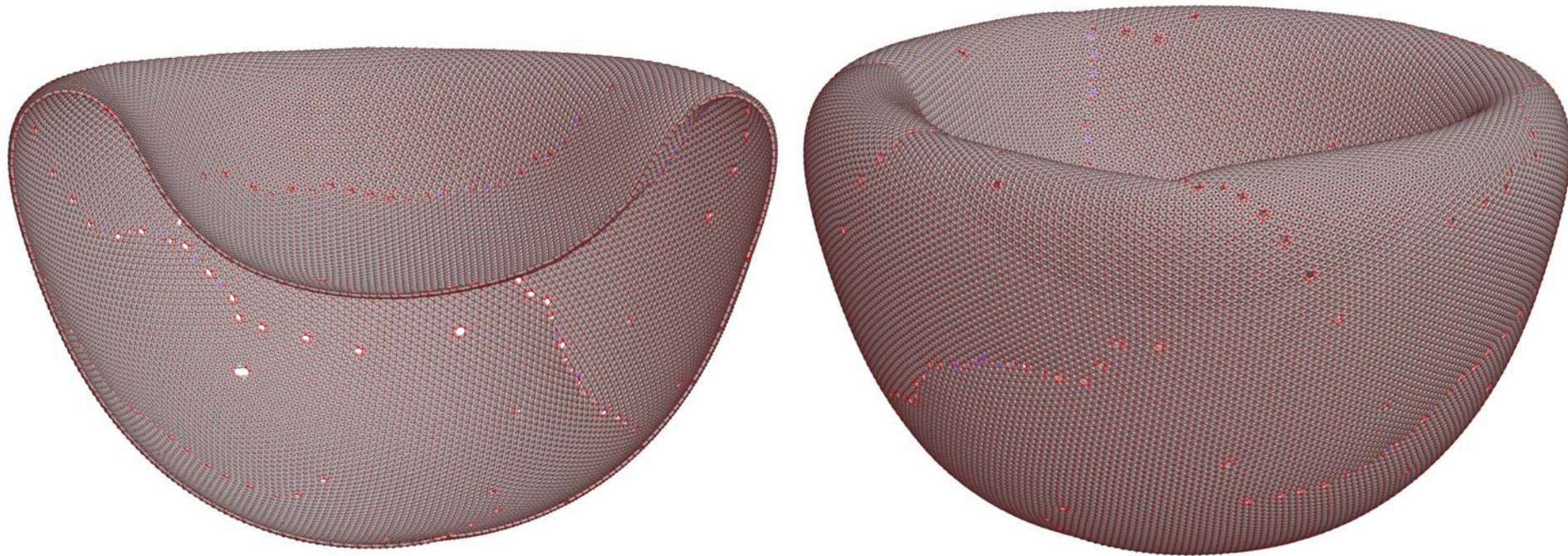
**GBs freely terminate!**

Images removed due to copyright restrictions.

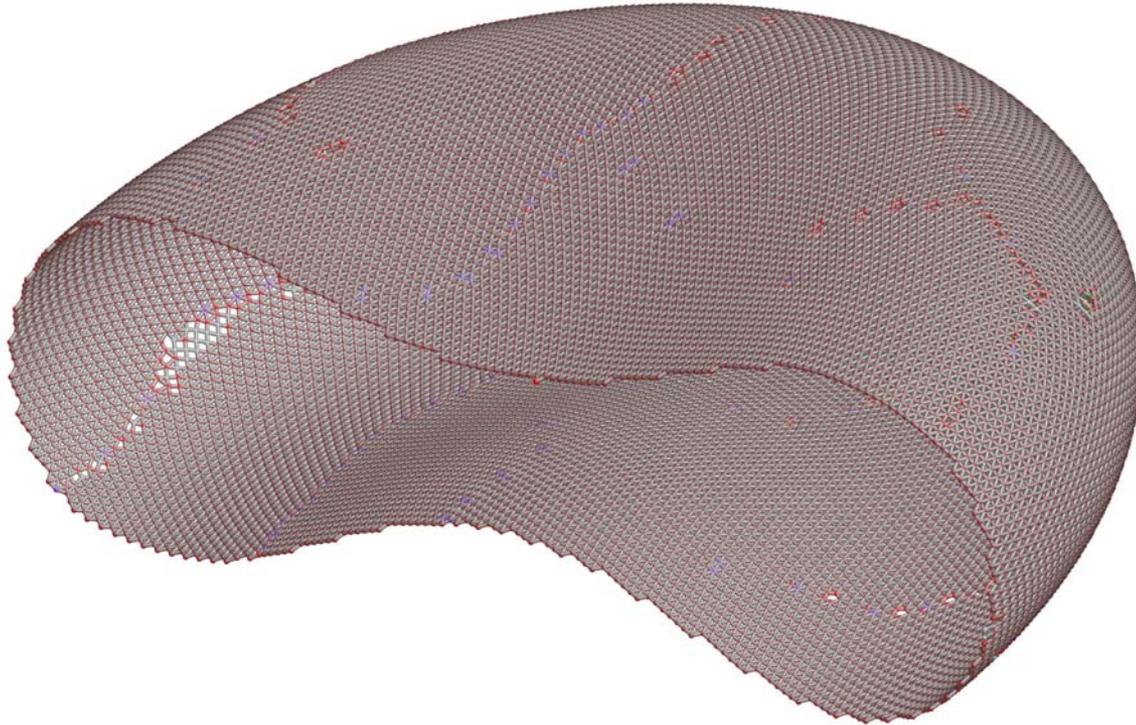
See Fig. 1 in Bausch, et al. "Grain Boundary Scars and Spherical Crystallography." *Science* 299 (2003): 1716-1718.

These GBs should be widespread in nature: large viral protein capsids, giant spherical fullerenes, spherical bacterial surface layers, siliceous skeletons of spherical radiolaria (aulosphaera), etc. Sites for chemical reactions, initiation points for bacterial cell division, influence the mechanical response.

# Material reference state for the in-plane shear energy $E_{\text{shear}}$



60% volume: **spherical state** as stress-free reference.



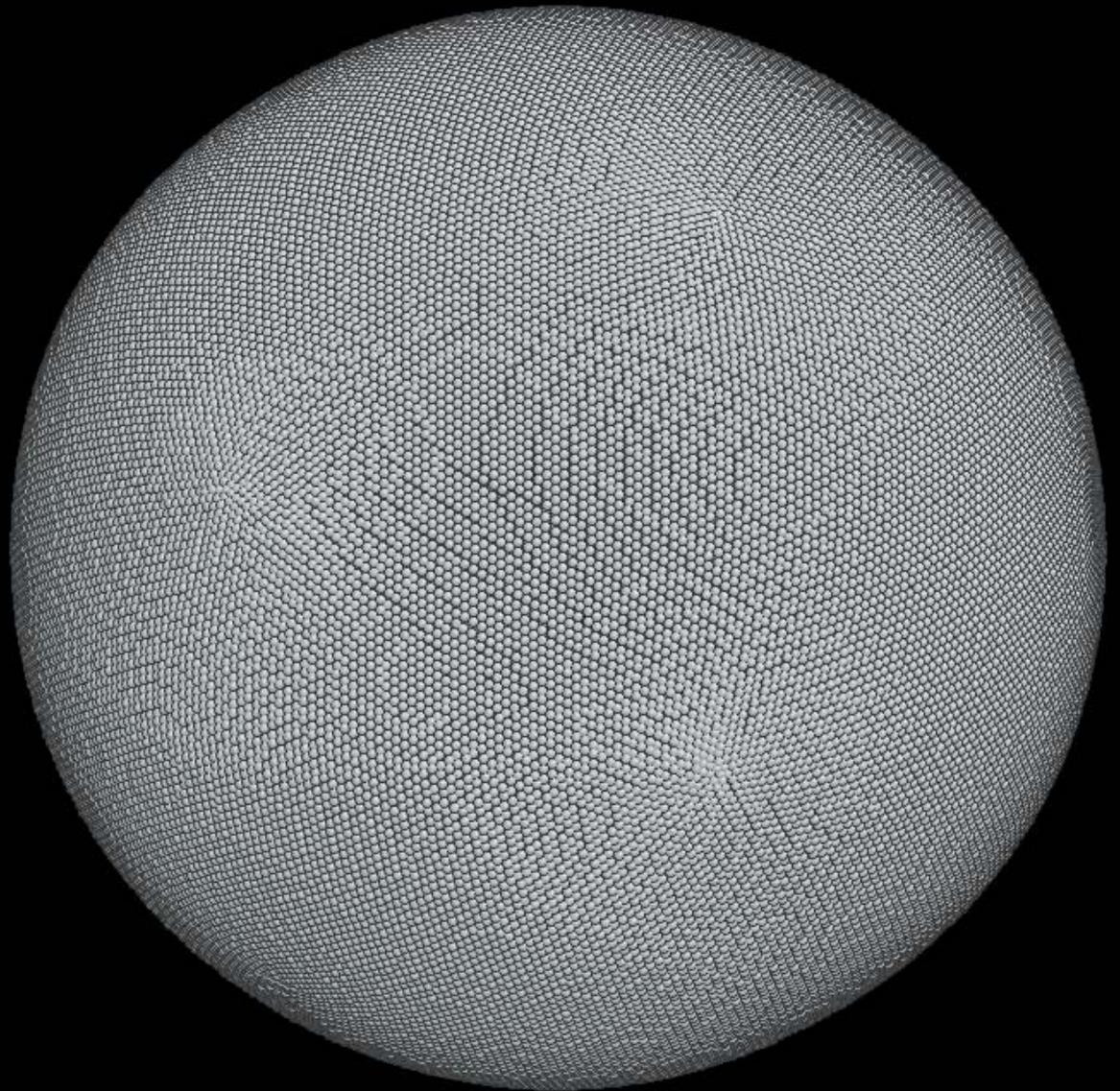
**W/ experimental range of parameters and sphere as stress-free reference state, the biconcave shape is only metastable at 60% volume.**

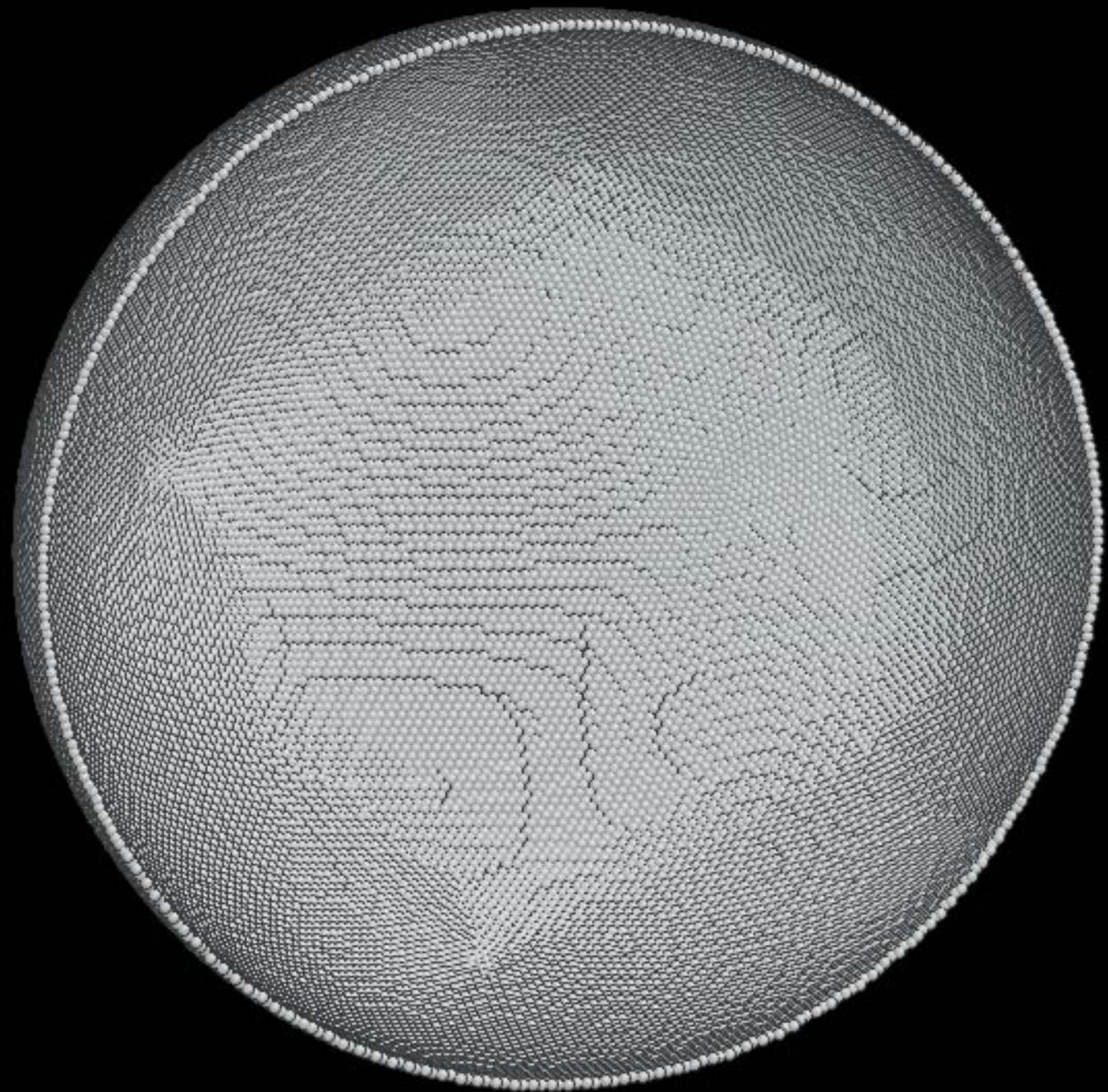
**With bending  
energy**

**$E_{\text{bend}}$  only**

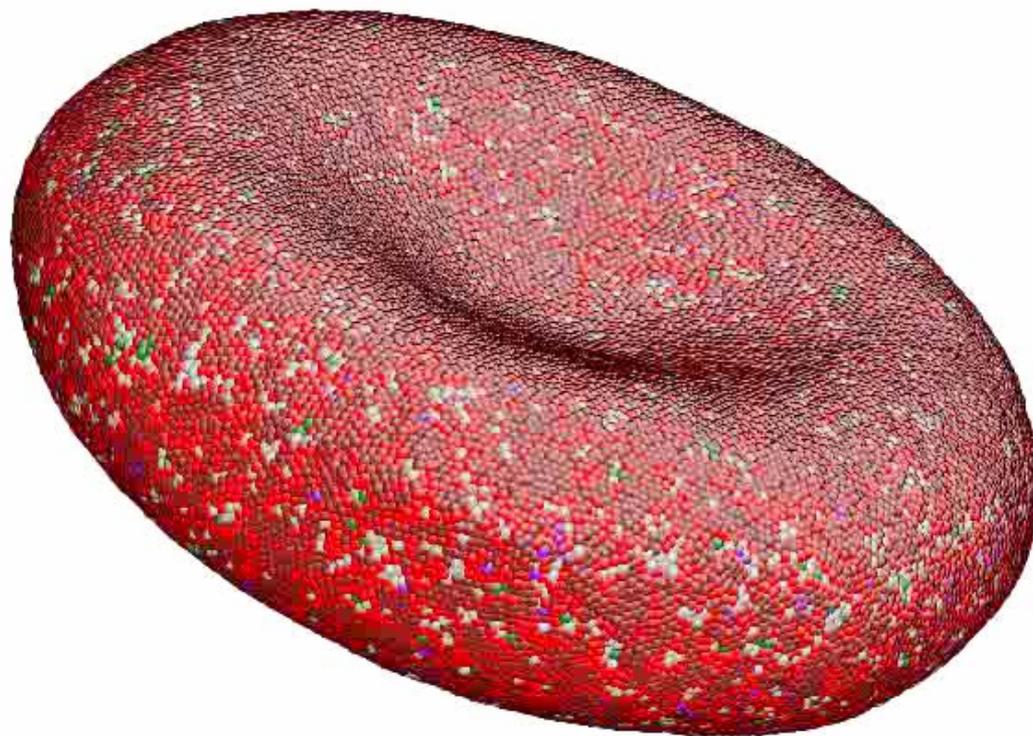
Canham (1970)

Helfrich (1973)

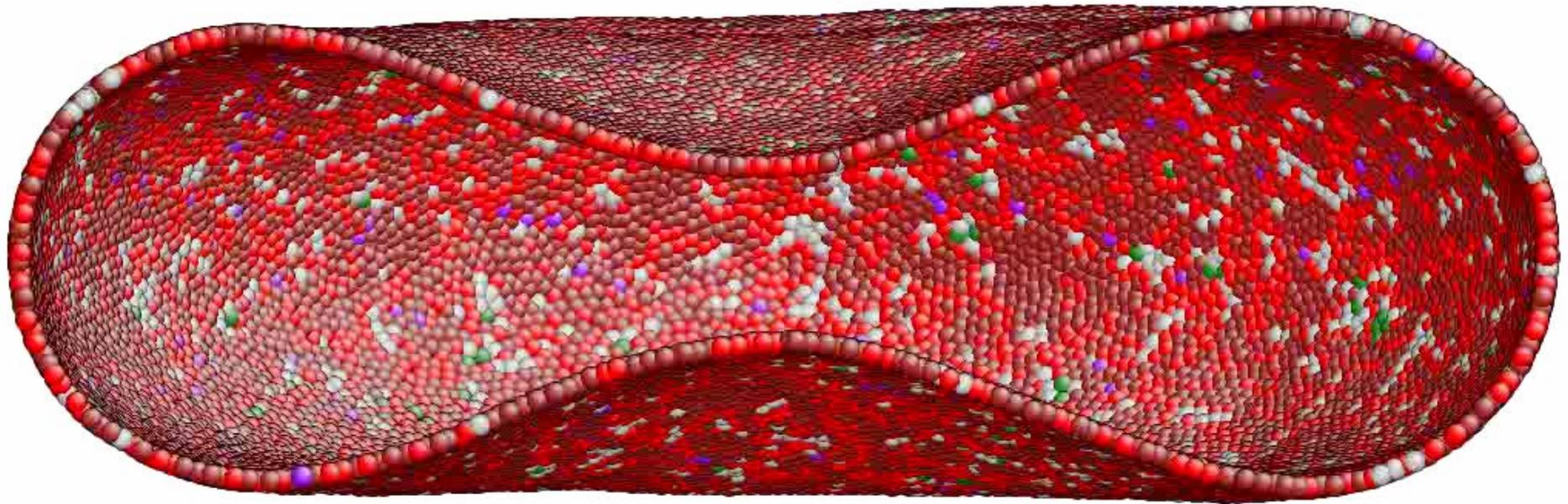


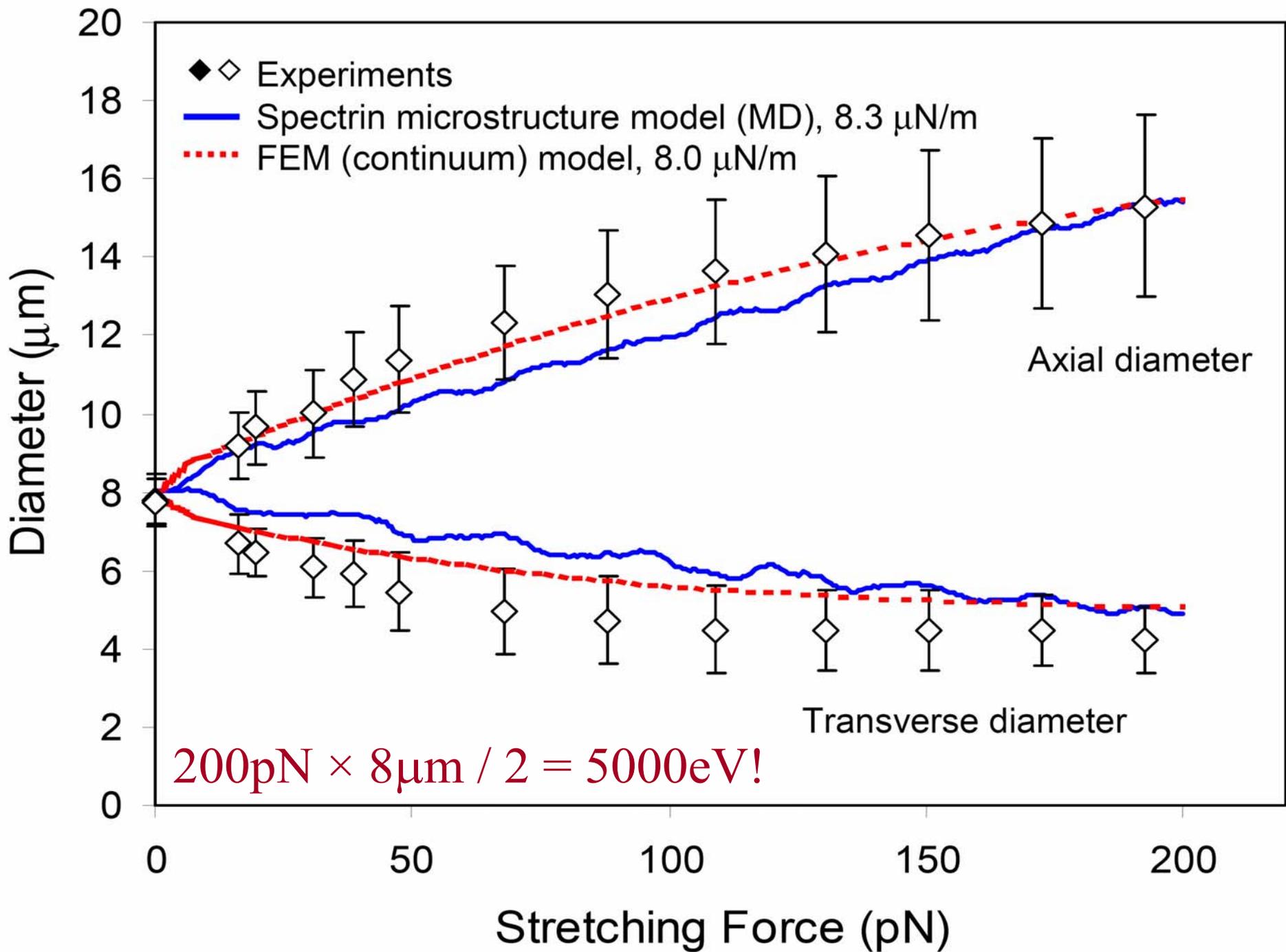


# Optical Tweezers Stretching Simulation

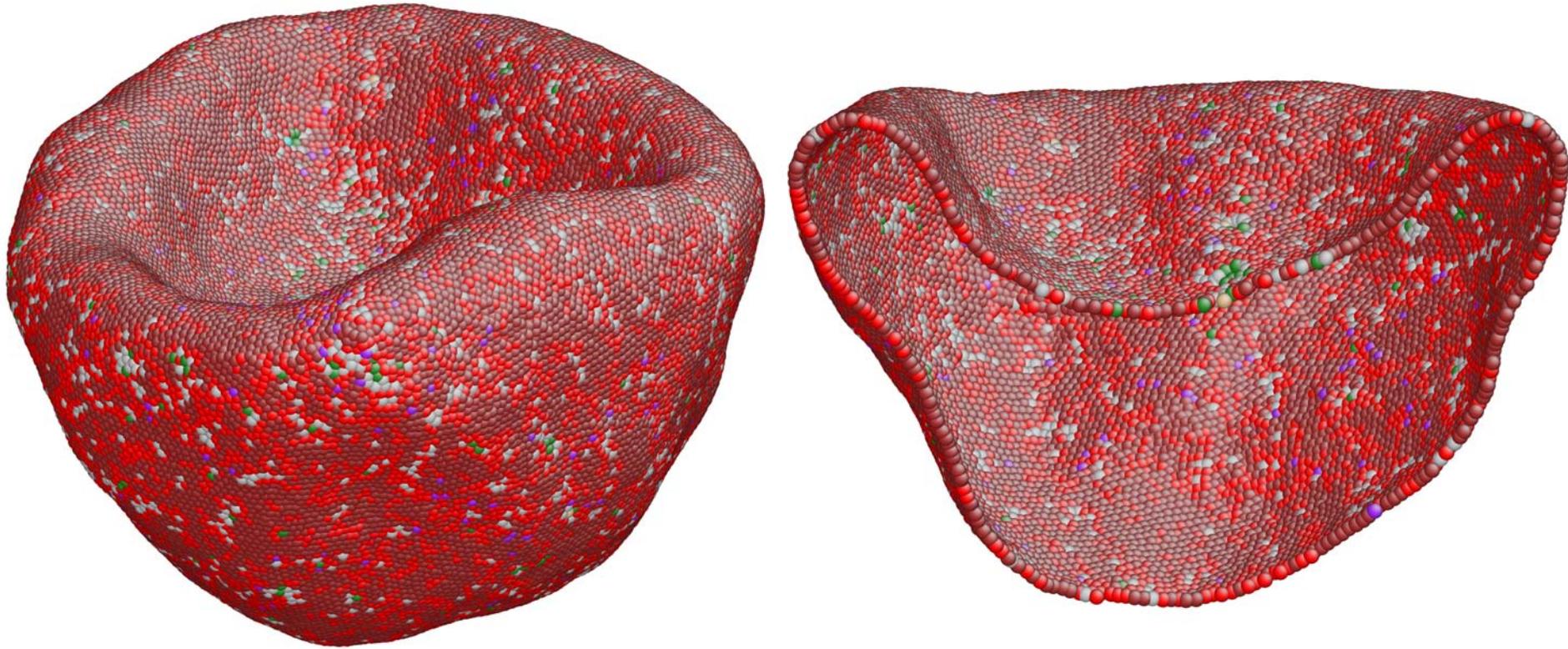


# Cross Sectional View





# Why is biconcave the stable equilibrium shape?



$$E_{\text{bend}} \sim 8\pi\kappa: \kappa \sim 2 \times 10^{-19} \text{ J} \rightarrow E_{\text{bend}} \sim 30 \text{ eV}$$

$$E_{\text{shear}} \sim \mu\varepsilon^2 A: \mu \sim 8 \mu\text{N/m}, \varepsilon \sim 0.1, A \sim 140 \mu\text{m}^2 \\ \rightarrow E_{\text{shear}} \sim 70 \text{ eV}$$

# Material Concept Hypothesis

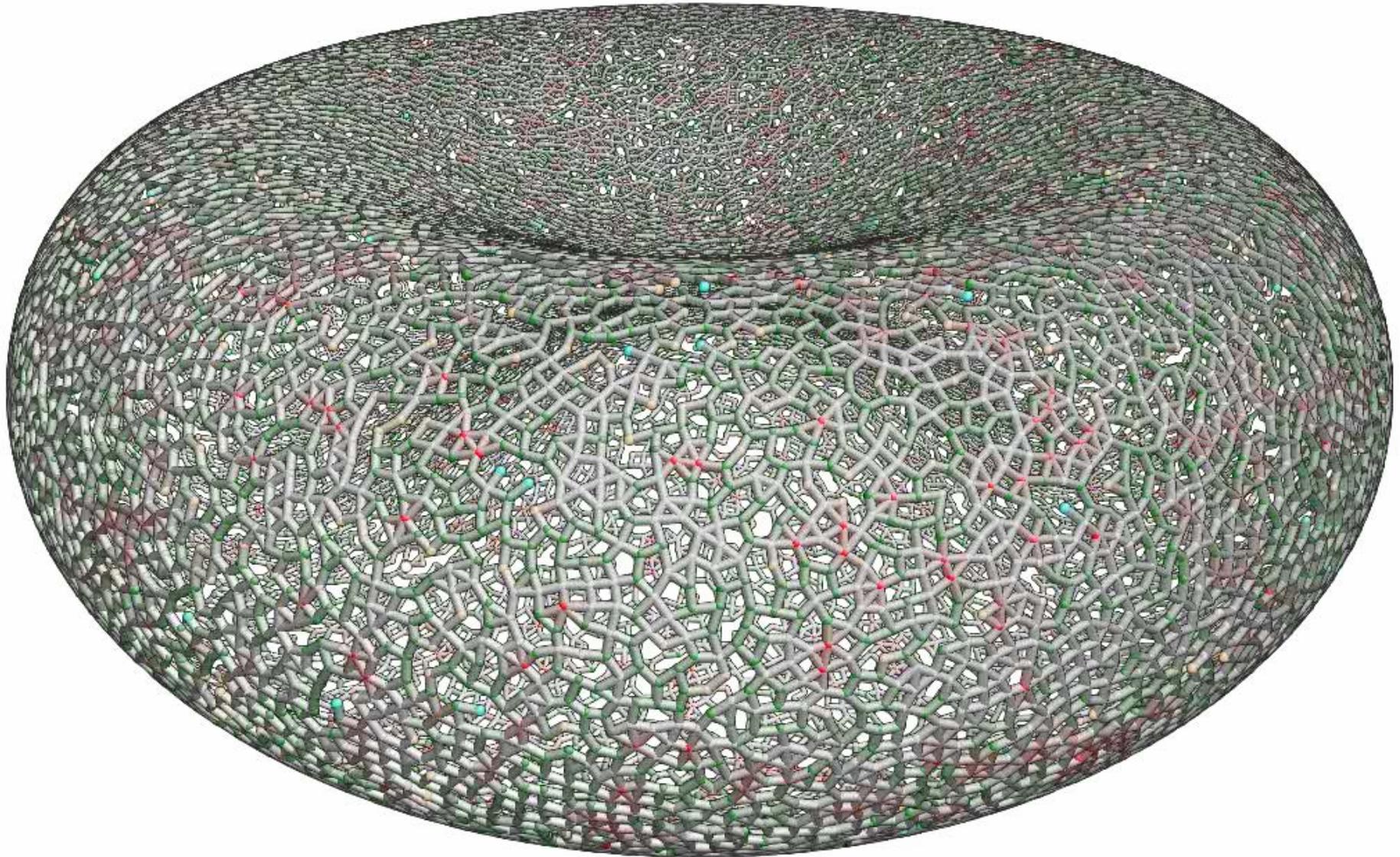
Li, Dao, Lim & Suresh, *Biophys. J.* **88** (2005) 3707.

- In an ideal limit, for any RBC shape, the cytoskeleton will always undergo remodeling in topological connectivity at a slow rate to relax its in-plane *shear* elastic energy to *zero*.

“liquefaction”, “slow-flowing glass”

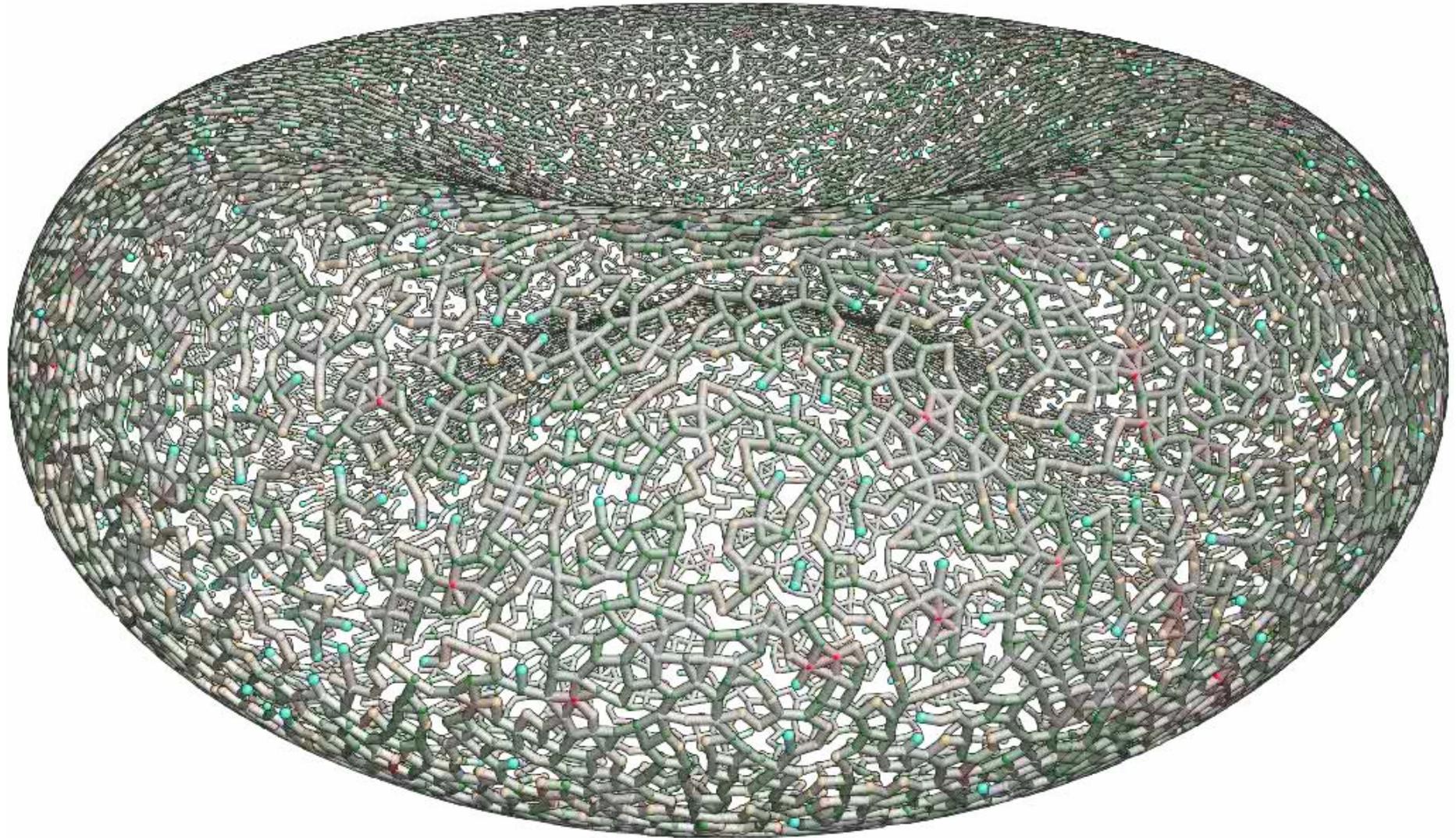
- At the timescale of optical tweezers stretching, the above relaxation is not significant, so large shear energy can be injected temporarily.

# Stillinger-Weber liquid on curved surface:



**no shear energy can survive long!**

# RBC cytoskeleton at reduced spectrin density



**very large holes start to percolate ...**

# Extreme Statistics of Cytoskeletal Defects in RBC

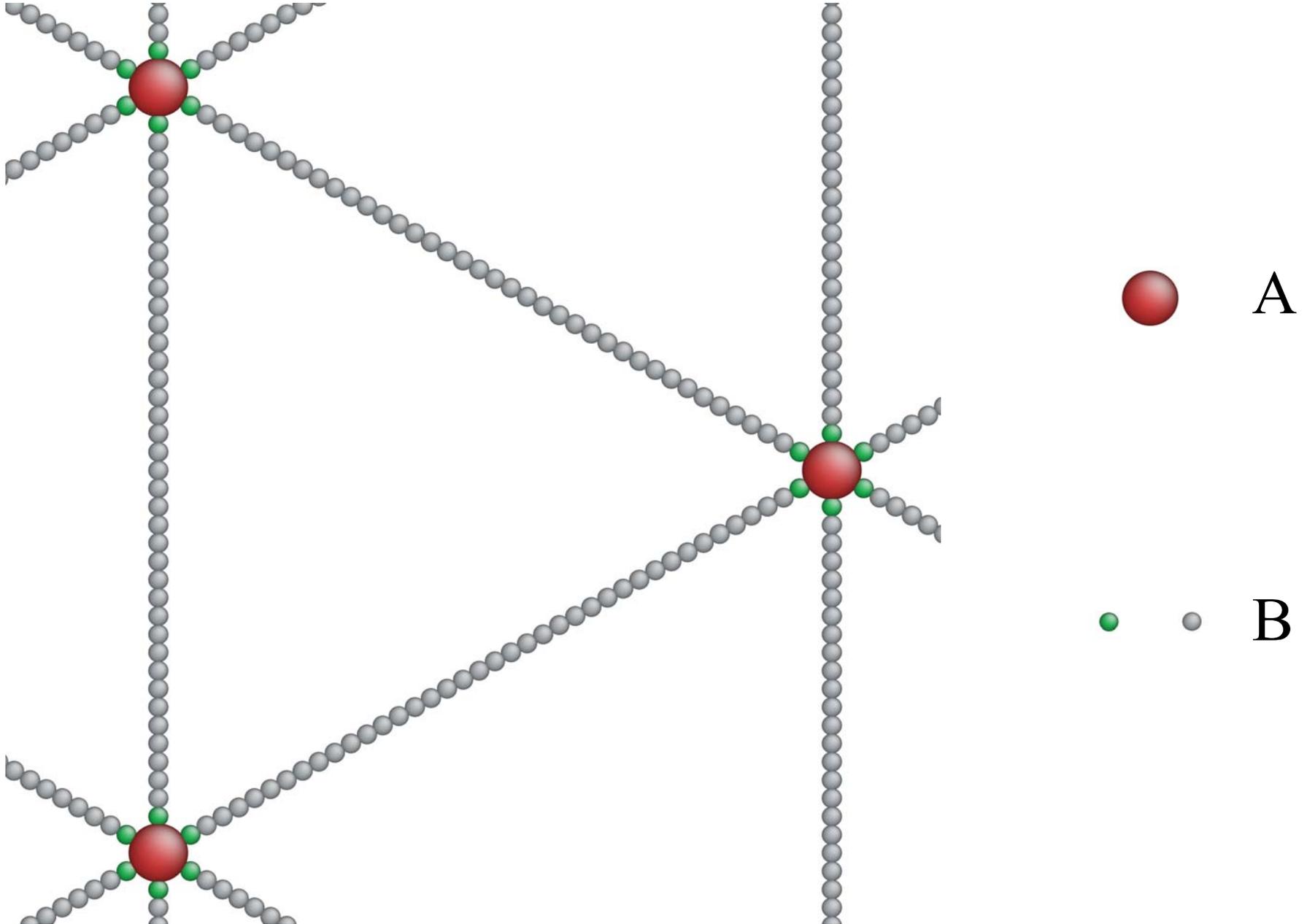
	actin#	spectrin#	largest polygon hole
normal	28673	81718	6
degree-4.5	26880	57523	8
degree-4	24372	48012	11
degree-3.5	21504	37416	22
degree-3	18637	26837	35

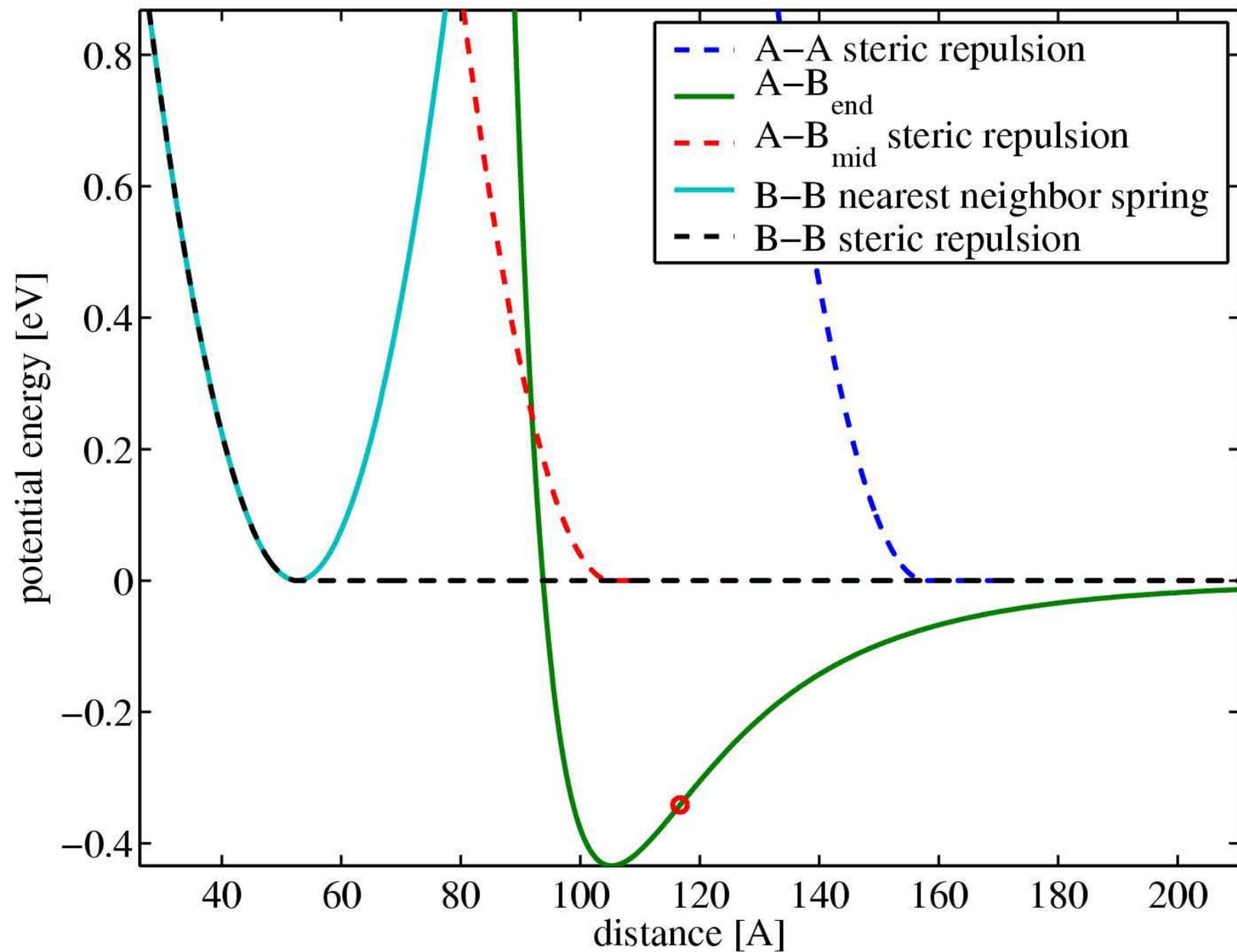
But this is basically from a “geometrical” simulation  
no biophysical basis, yet.

# Intermediate Summary

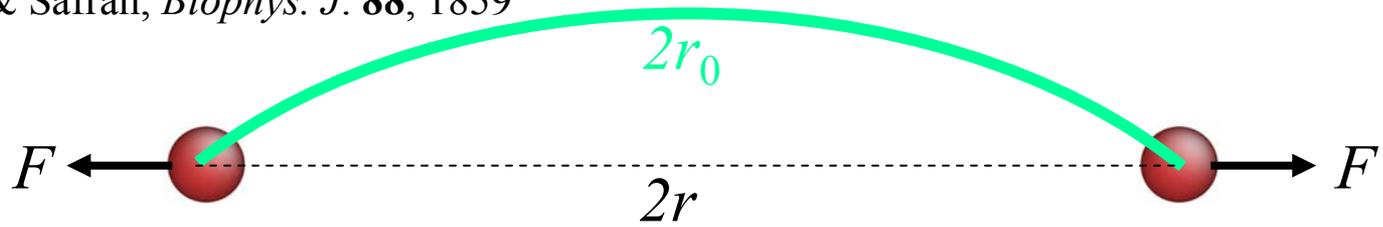
- Spectrin-level and continuum FEM analyses indicate our optical tweezers experiments give approximately the same in-plane shear modulus as micropipette aspiration experiments:  $\mu = 5 \text{ to } 10 \times 10^{-6} \text{ N/m}$ .
- Stabilization of biconcave equilibrium shape strongly suggests the cytoskeleton undergoes slow but constant remodeling topologically to always relax the in-plane shear elastic energy to zero.
- Connection to single-molecule stretching experiments (“intermolecular potential development”).

# CGMD model with *breakable* actin-spectrin junction



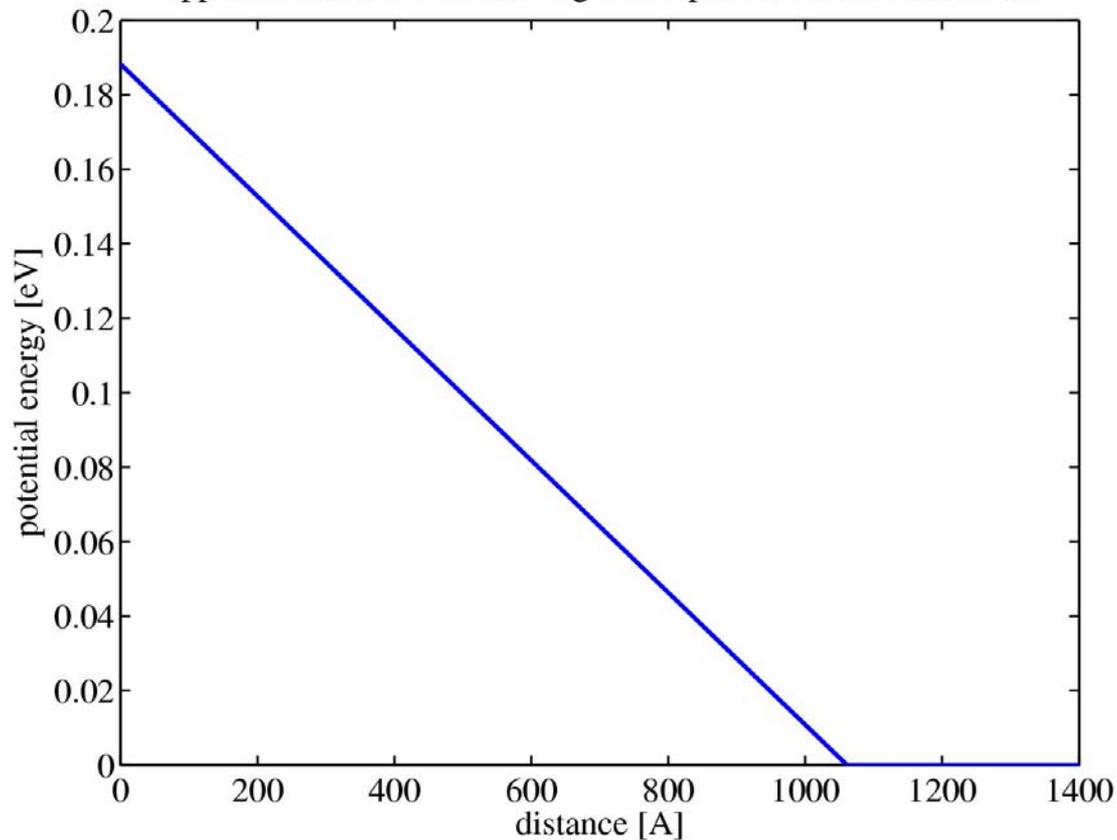


Reference: Gov & Safran, *Biophys. J.* **88**, 1859  $\kappa_{\text{bare}} = 2 \times 10^{-20}$  J

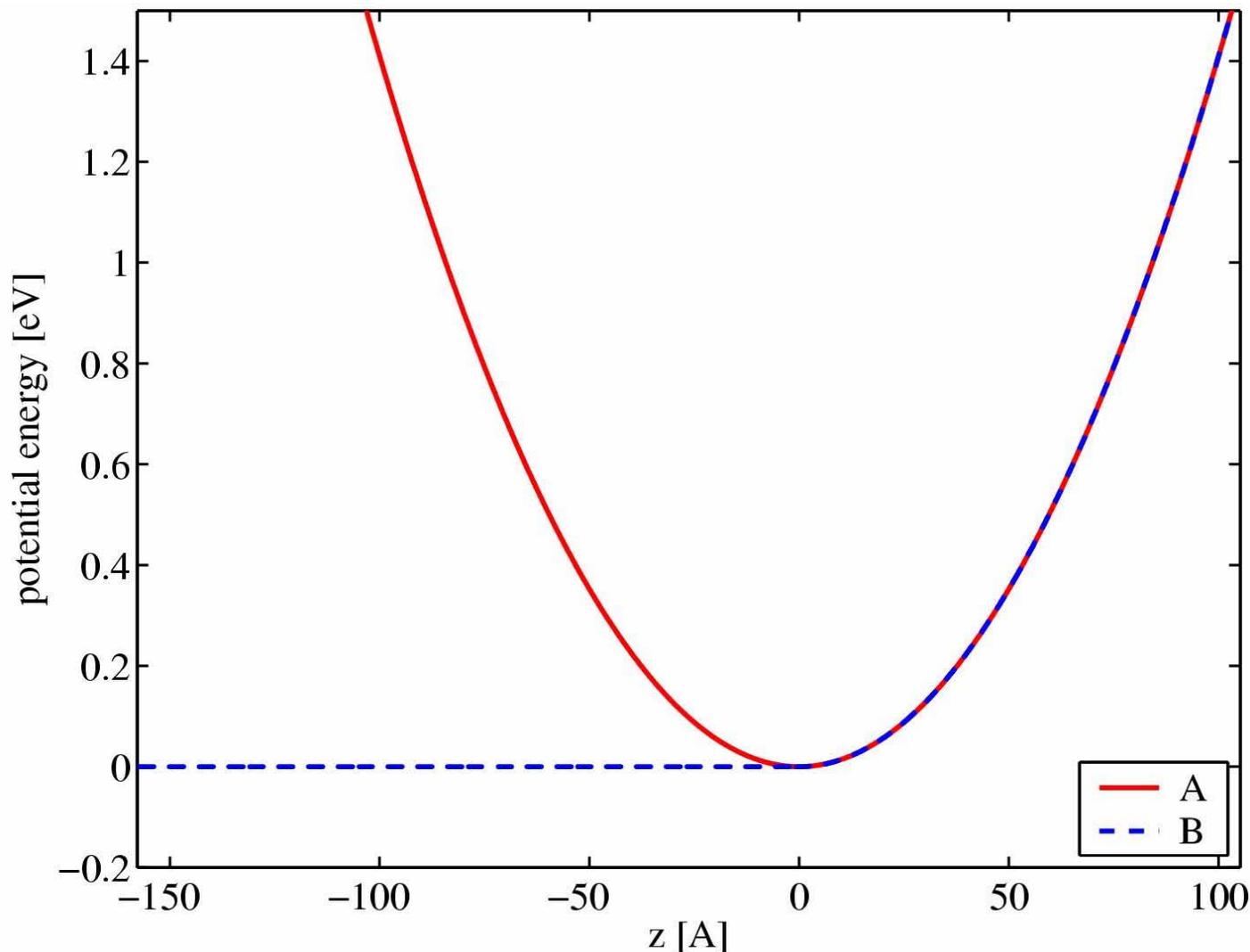


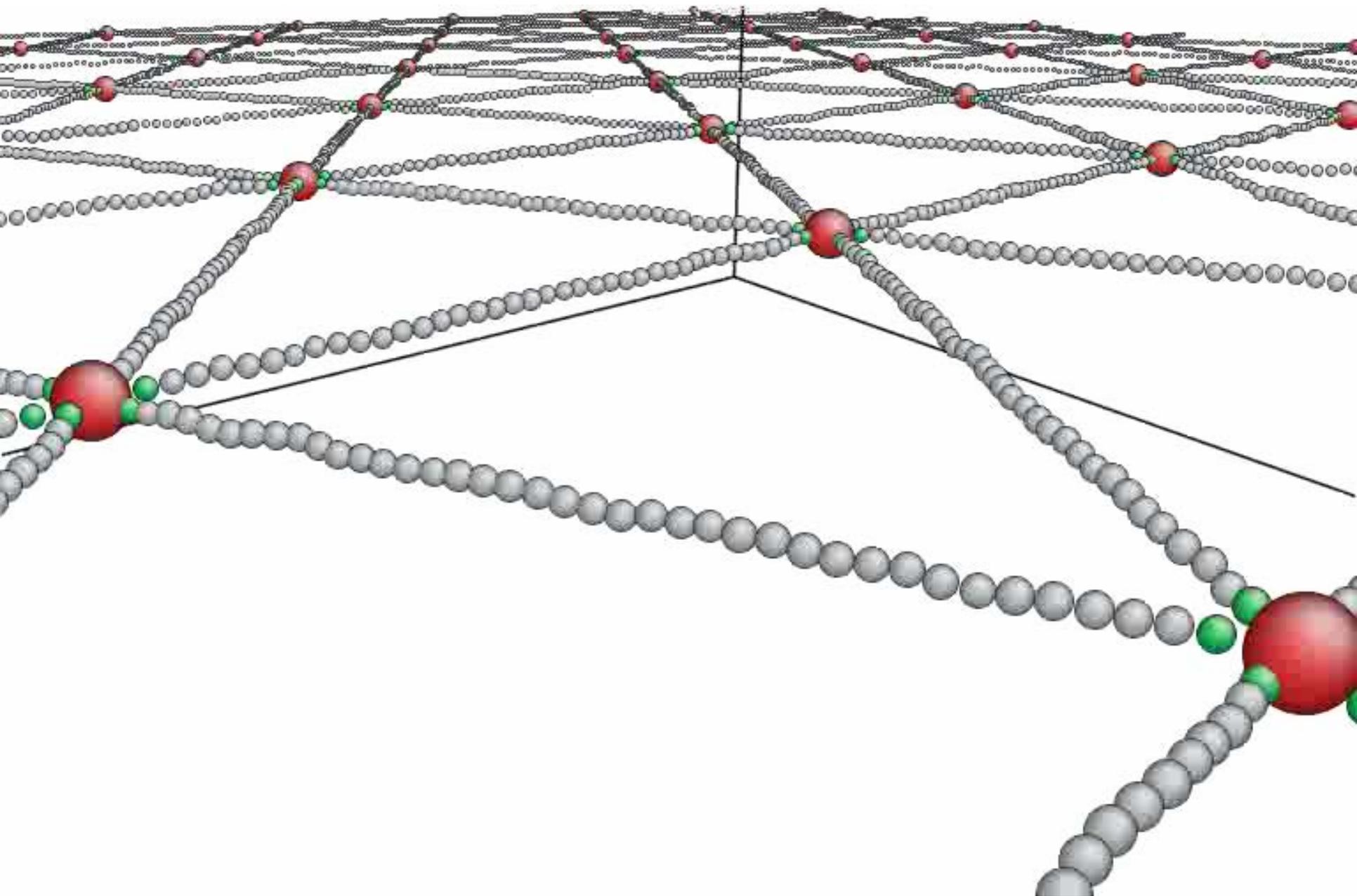
$$F = \alpha \frac{4\pi\kappa_{\text{bare}}}{3r_0}, \quad \alpha \text{ chosen to be } 0.36$$

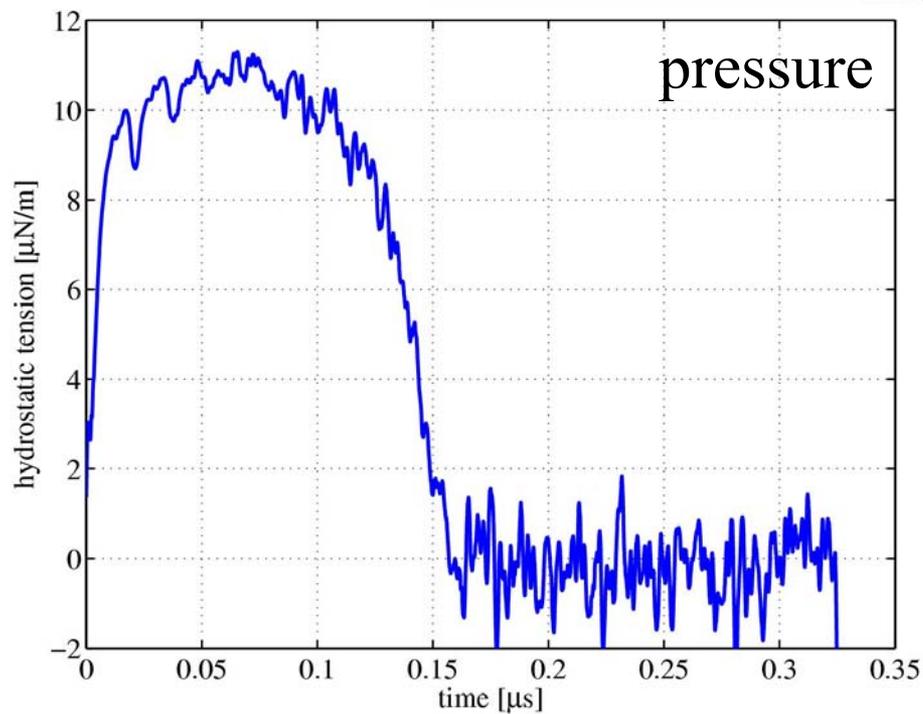
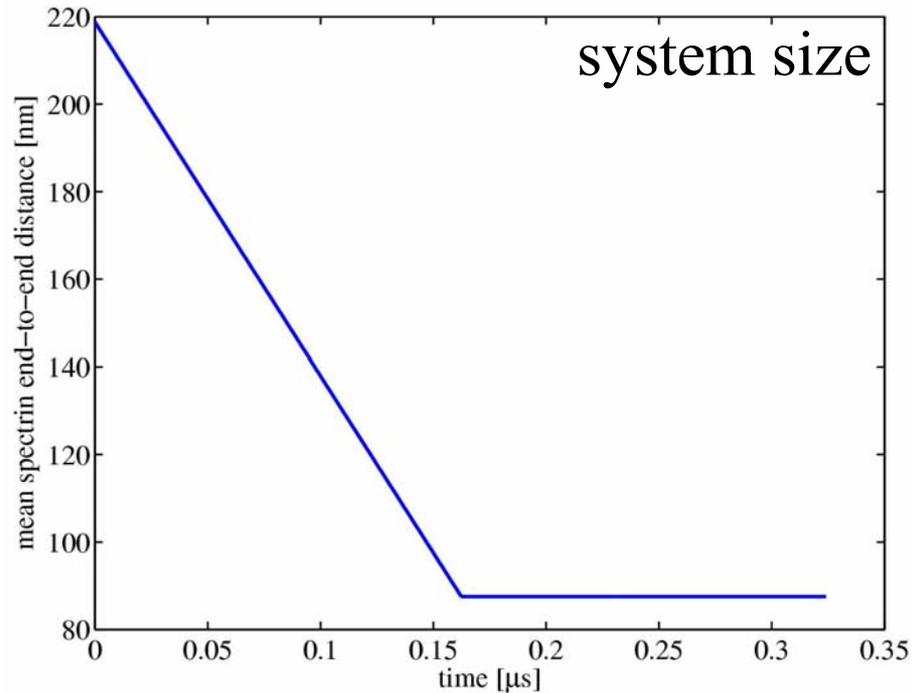
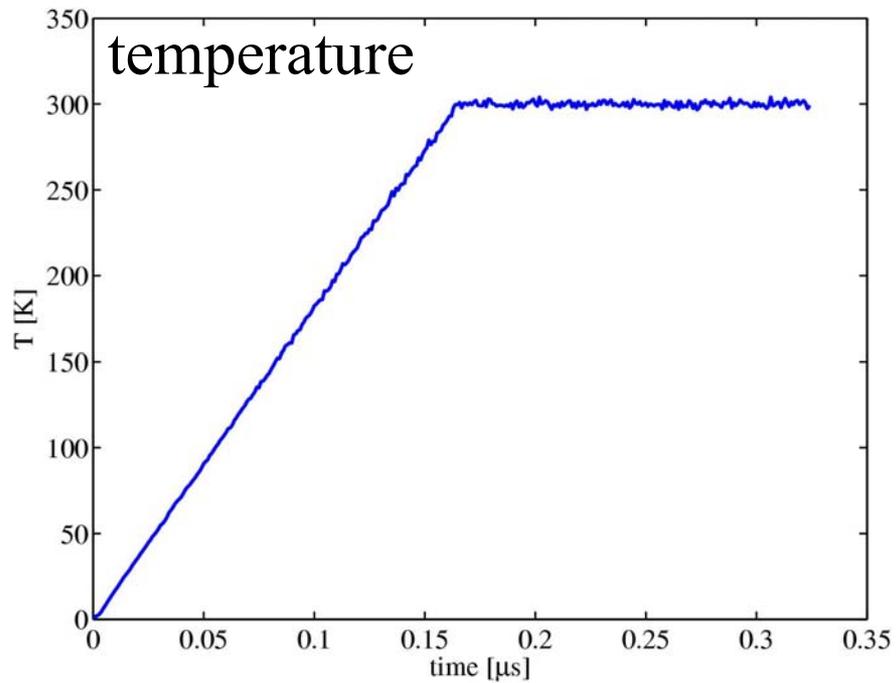
approximate A-A nearest neighbor repulsion due to membrane



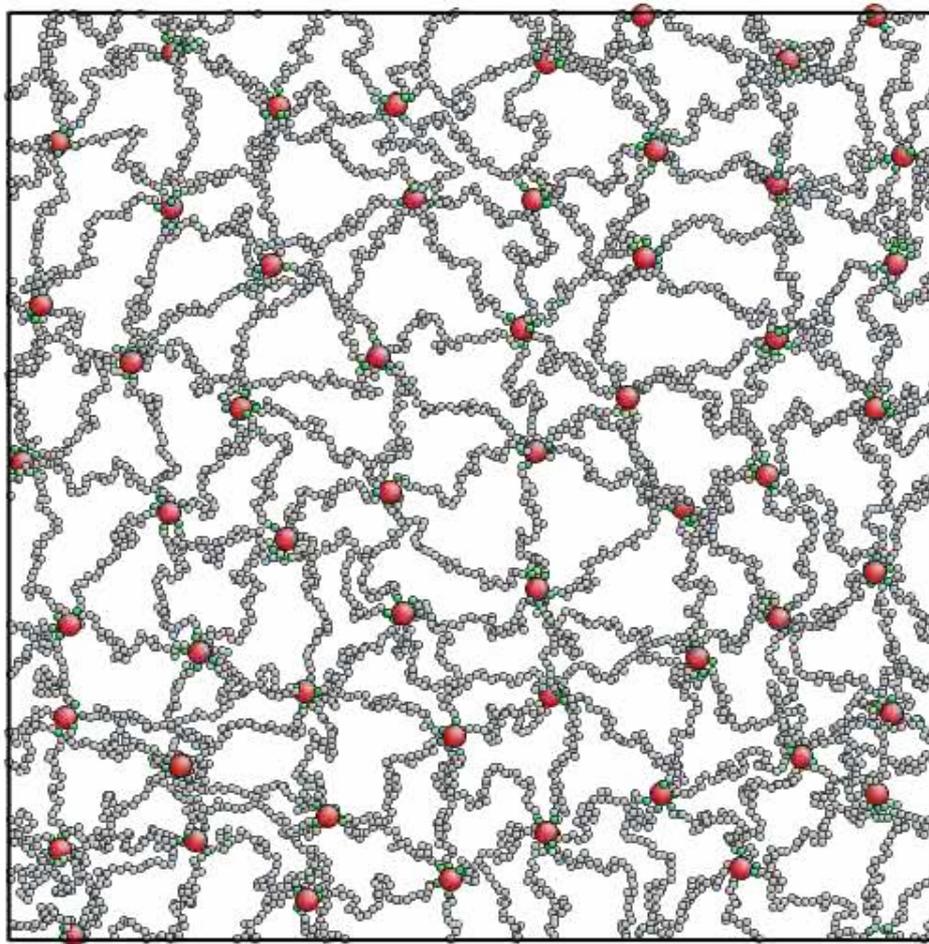
We also put soft ( $0.1k_{\text{BB}}$ ) confinement potential on A and B in  $z$  to mimic interaction with the membrane without actually simulating the membrane.



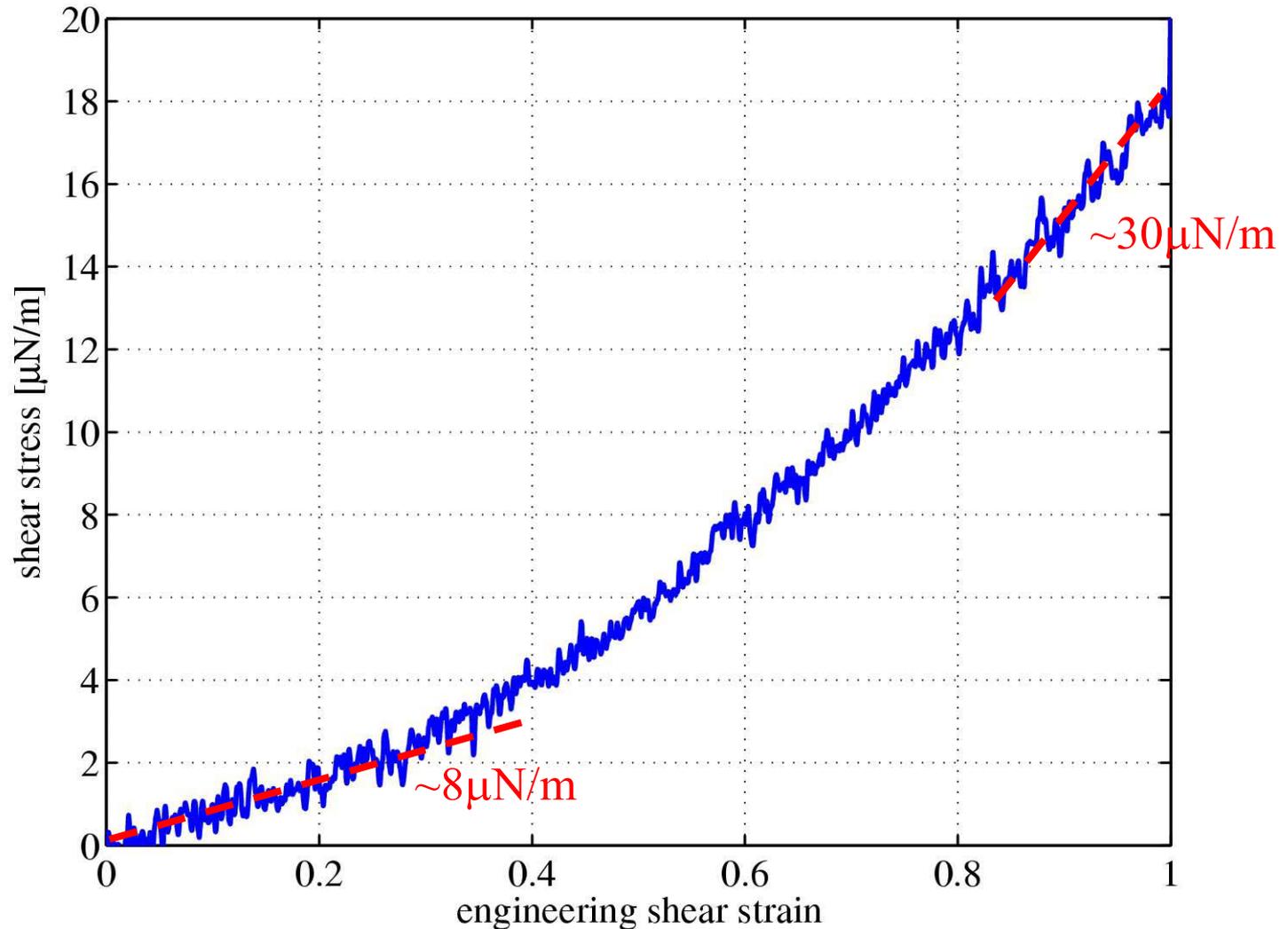




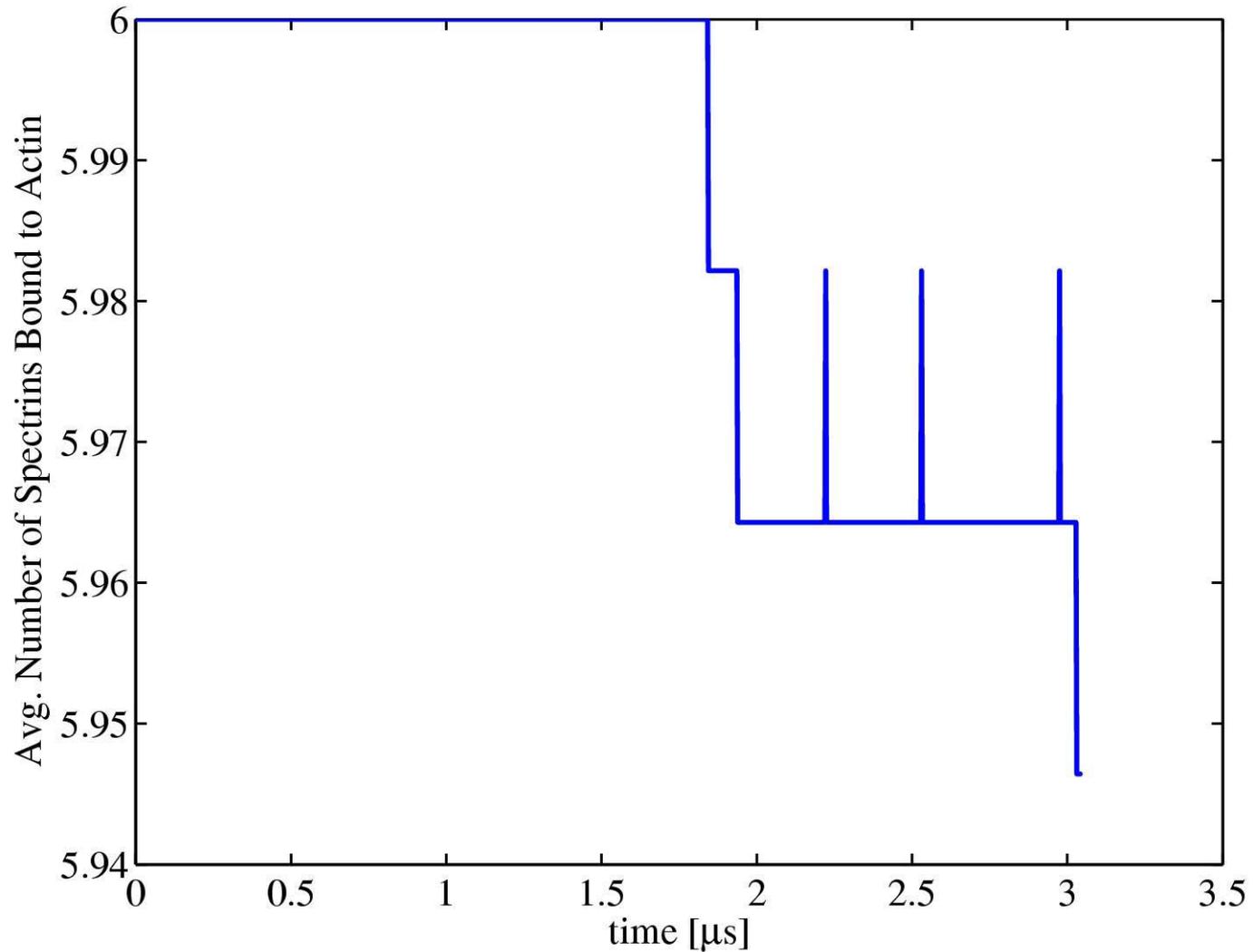
Pure shear deformation  
at 300K and strain rate  $3 \times 10^5/s$



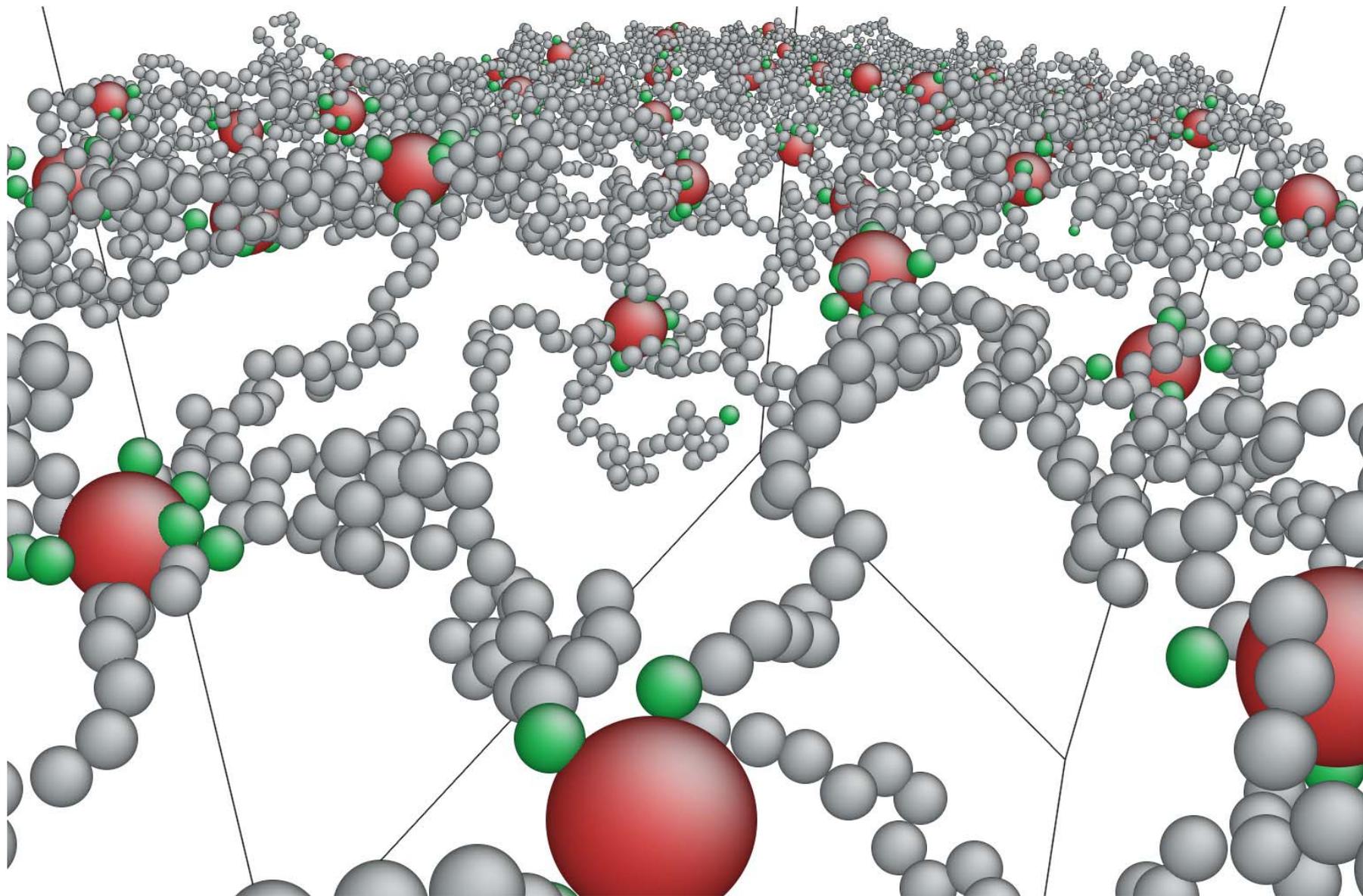
# Stress-strain curve at 300K and no ATP

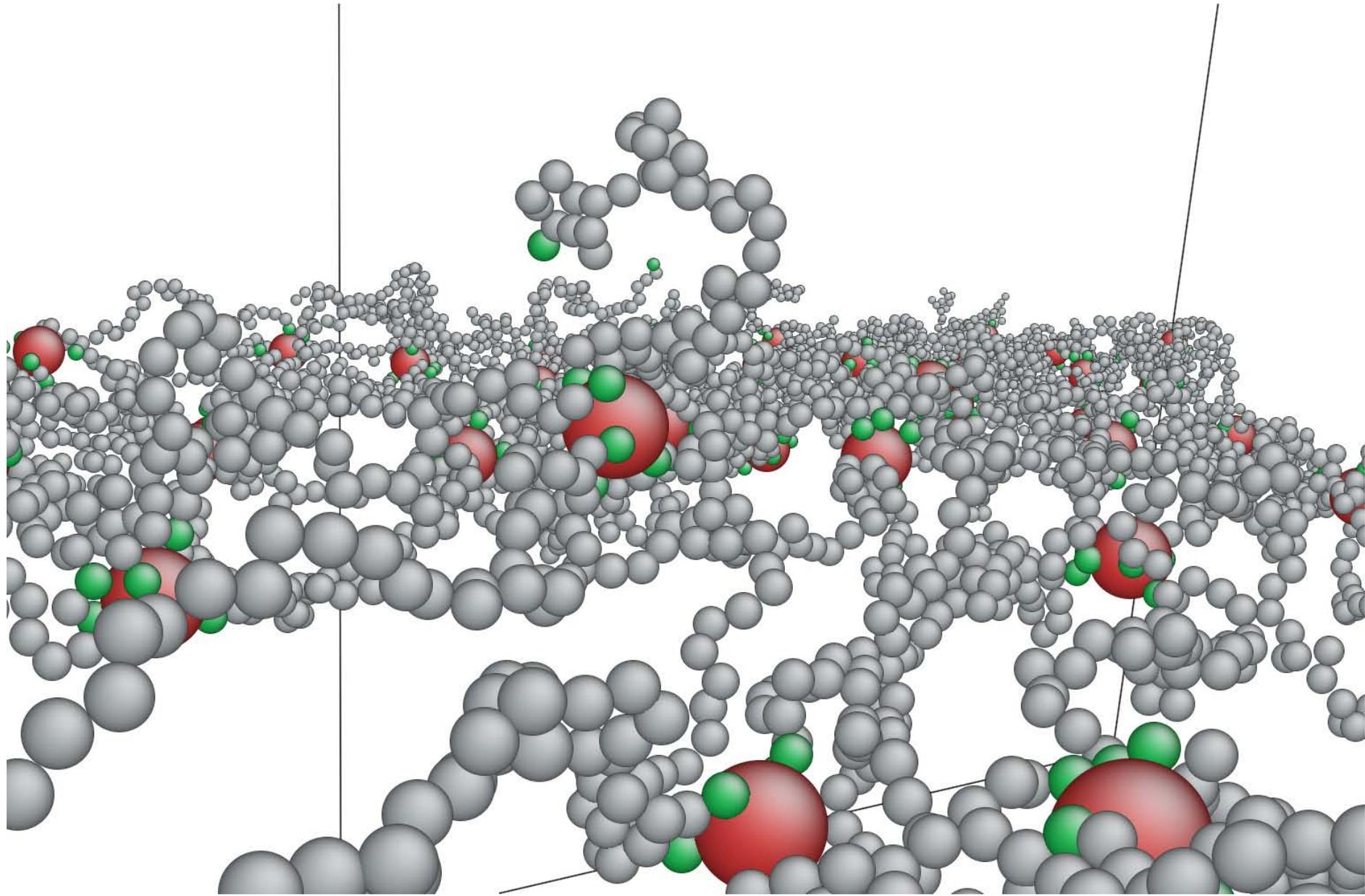


# Defect statistics at 300K with no ATP



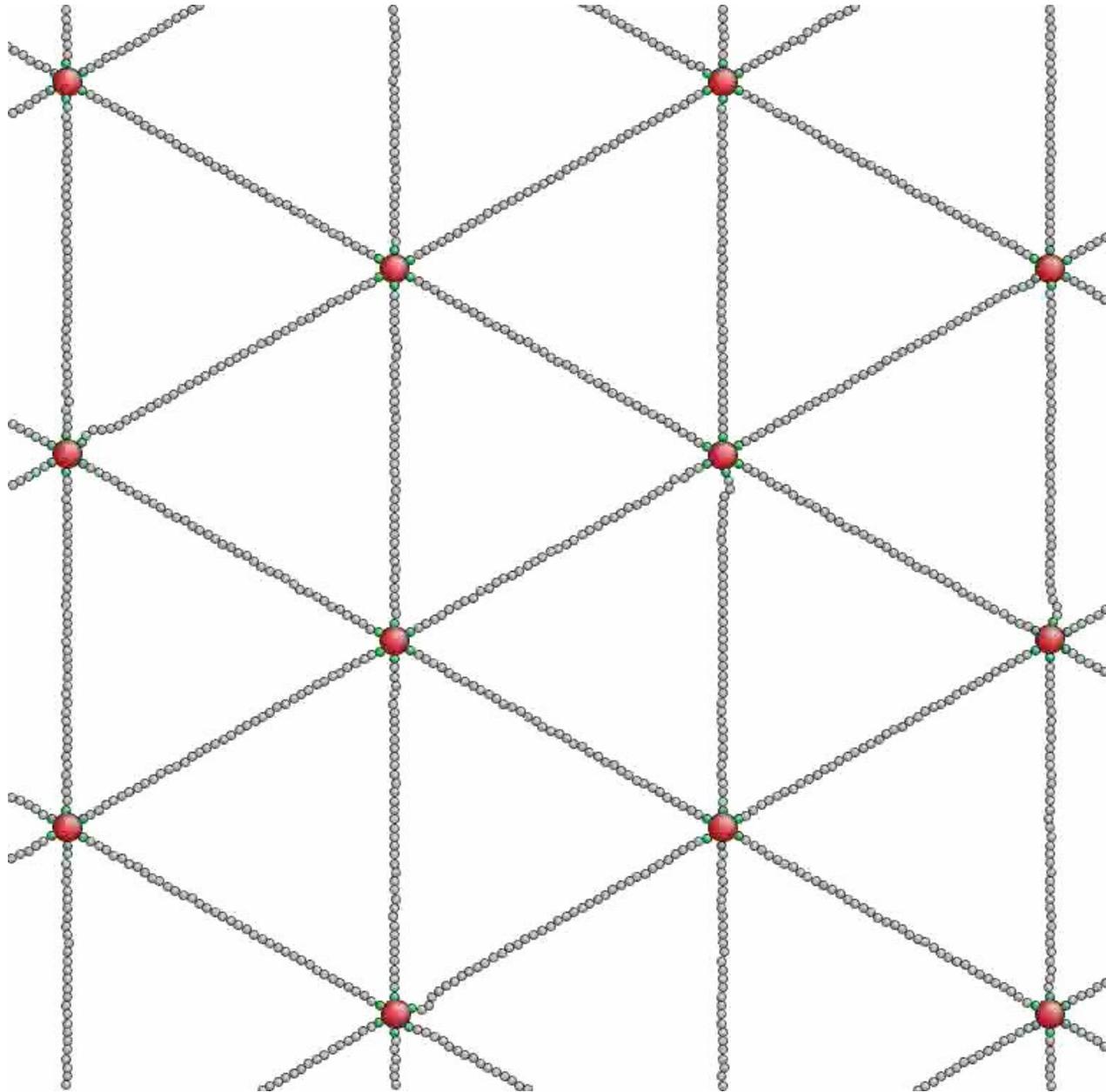
# A broken link 5-fold defect



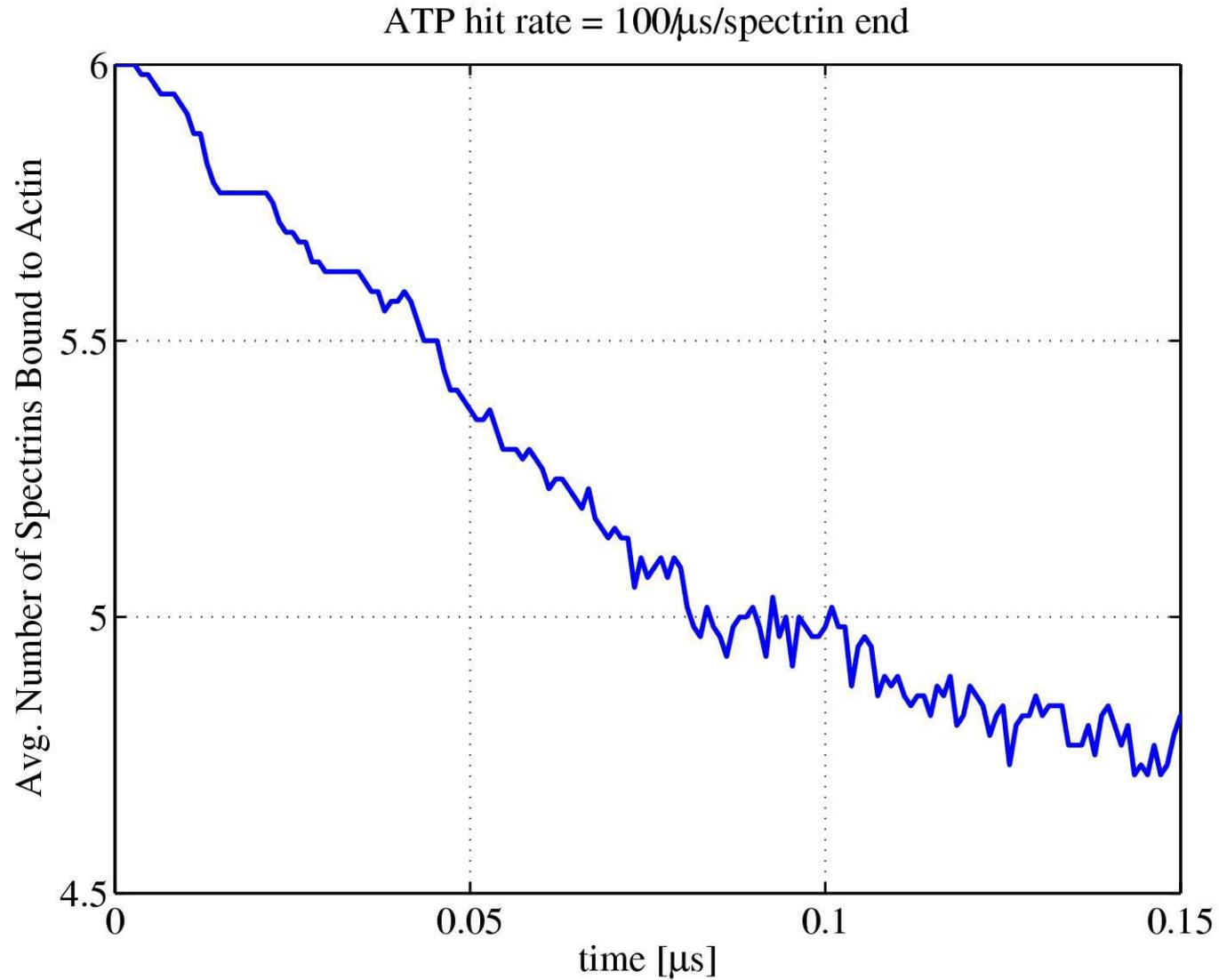


**Corrugation due to buckling: elevated / depressed in height**

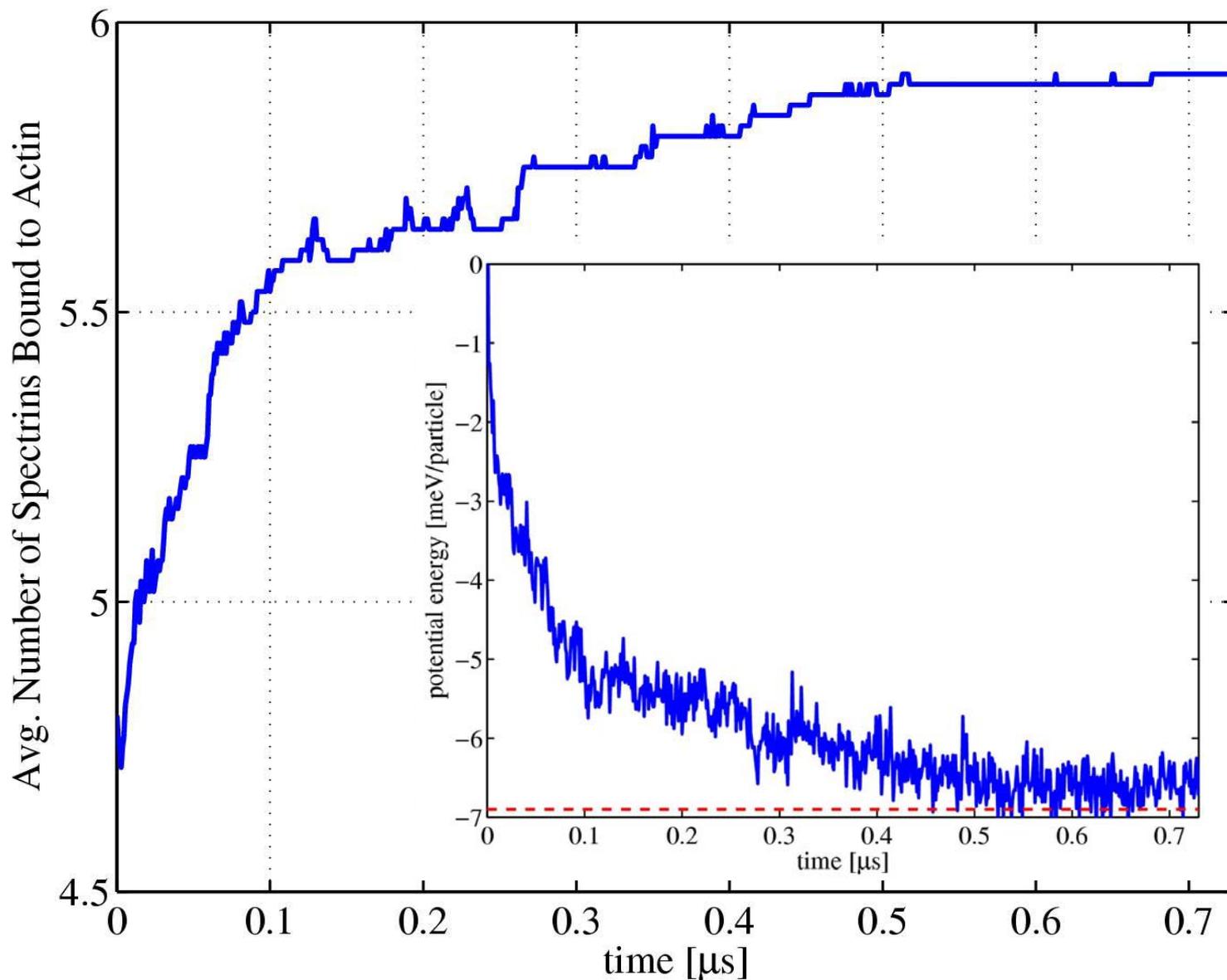
**Now add ATP (0.5eV random kinetic energy to green ball):**  
**hit rate = 100/ $\mu$ s per spectrin end**



# Defect statistics at 300K, ATP hit rate $100/\mu\text{s}$



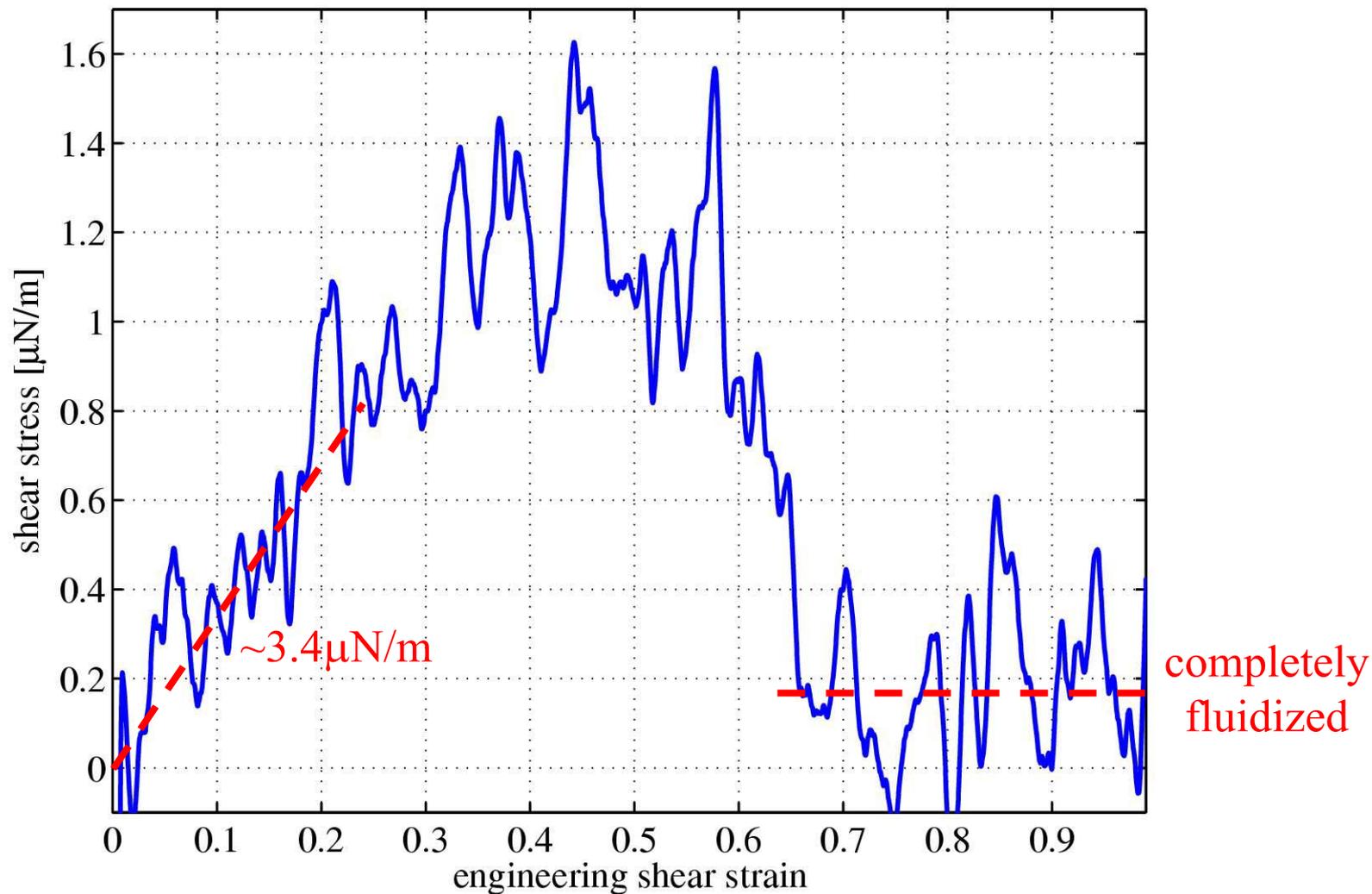
Now turn off ATP hits, “anneal” at 300K...



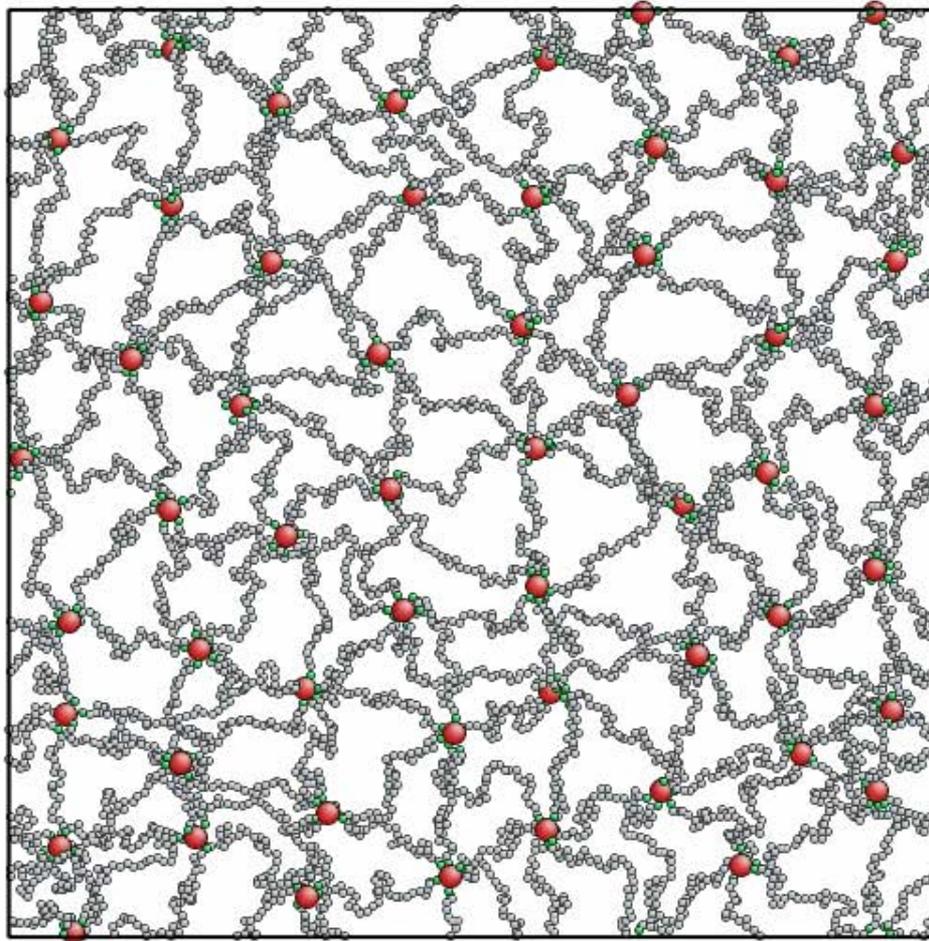
Miraculously, the system recovers, within CGMD simulation timescale.

A more reasonable ATP hit rate:  $10/\mu\text{s}$ .  
Simultaneously, also shear deform.

ATP hit rate =  $10/\mu\text{s}$ /spectrin, strain rate =  $3 \times 10^5/\text{s}$

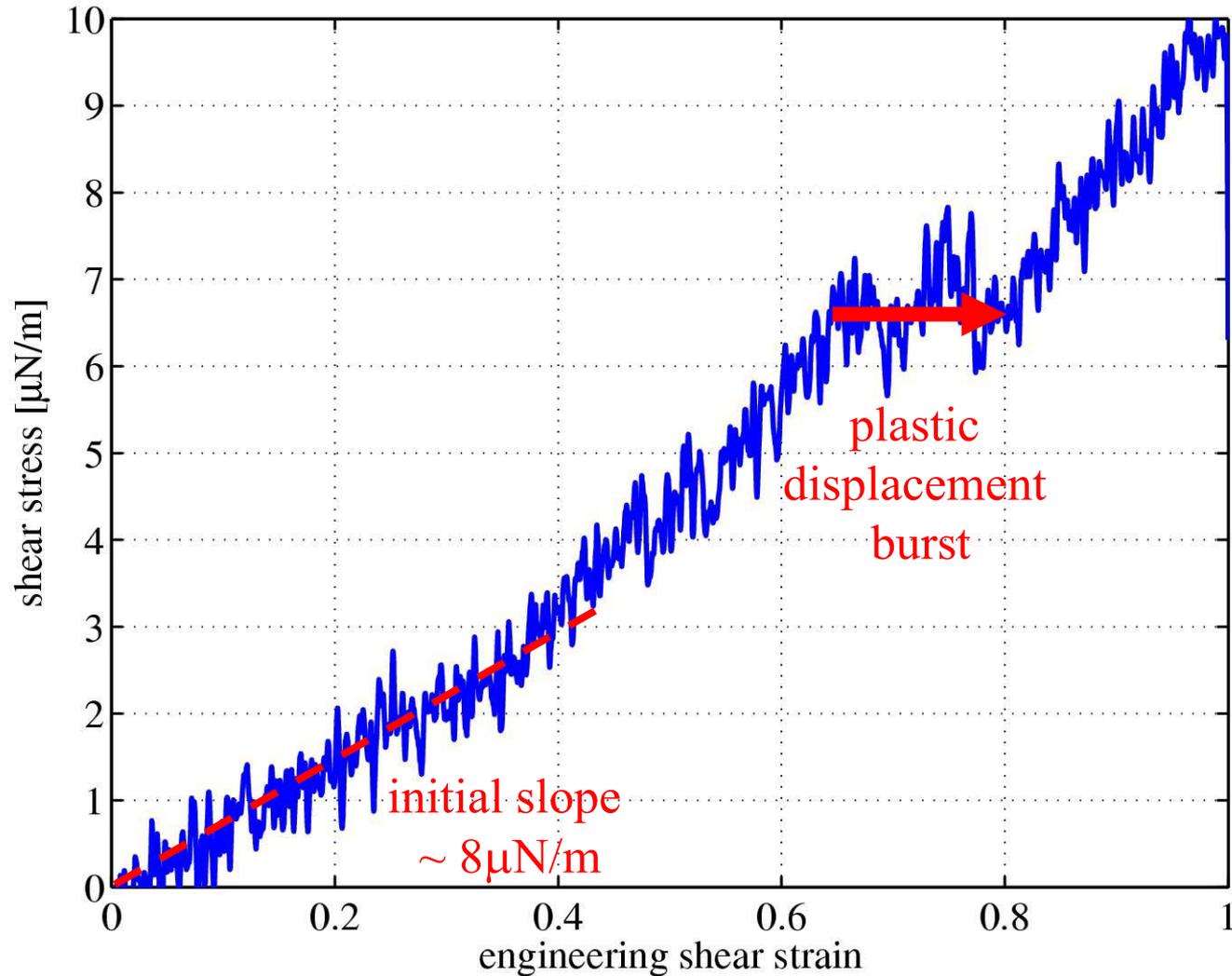


ATP hit rate =  $10/\mu\text{s}$

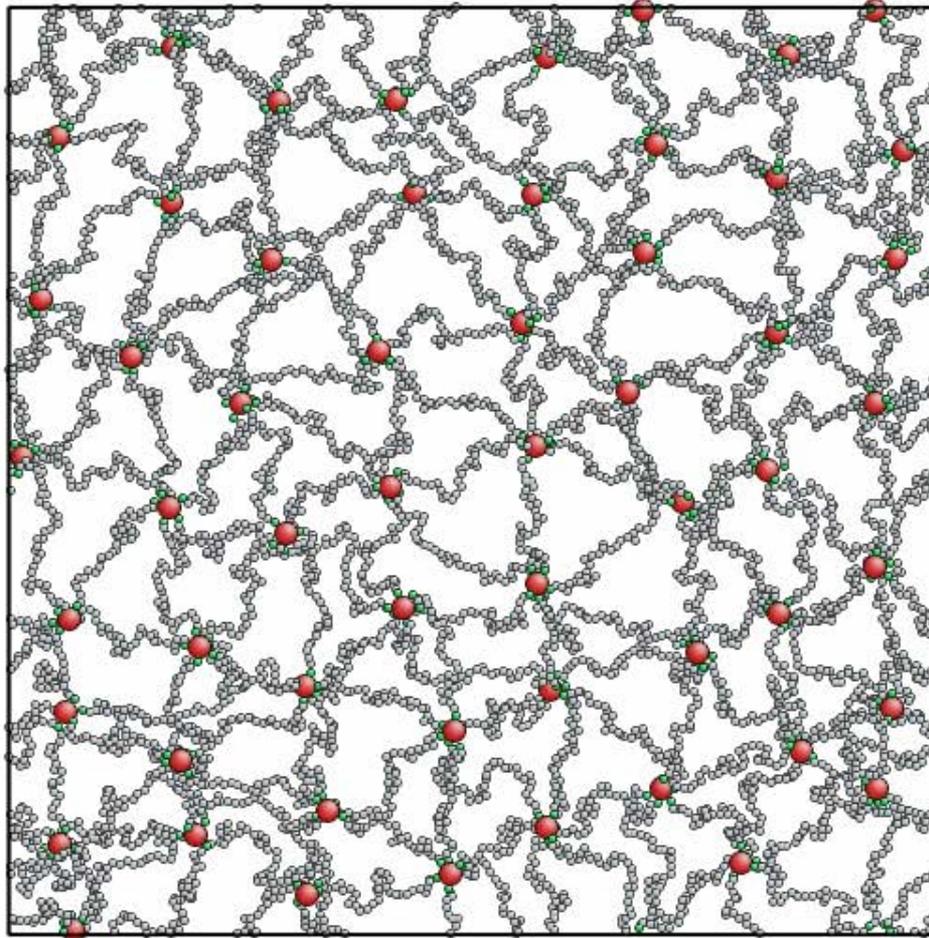


ATP hit rate =  $1/\mu\text{s}$ :

ATP hit rate =  $1/\mu\text{s}$ , strain rate =  $3 \times 10^5/\text{s}$

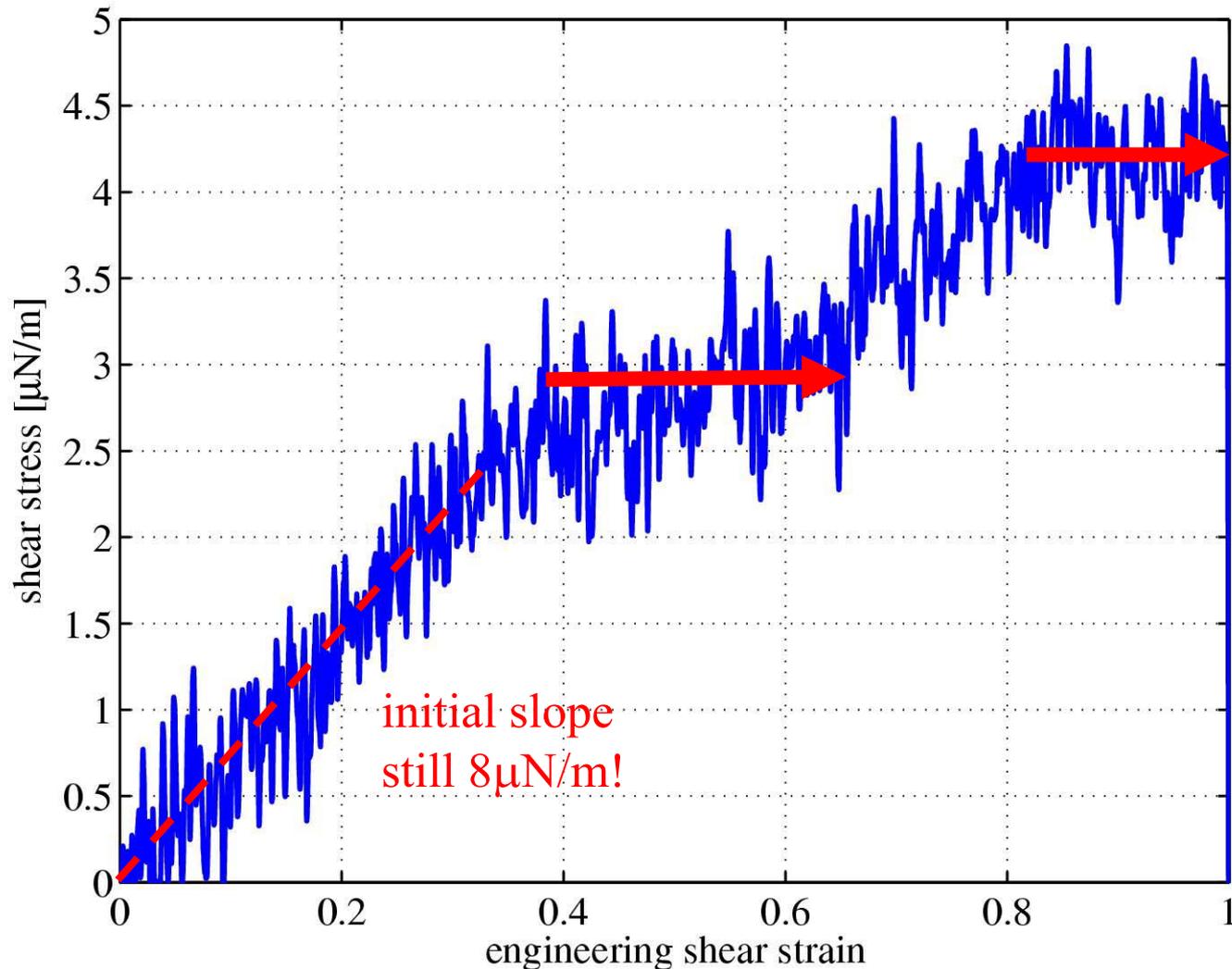


ATP hit rate =  $1/\mu s$

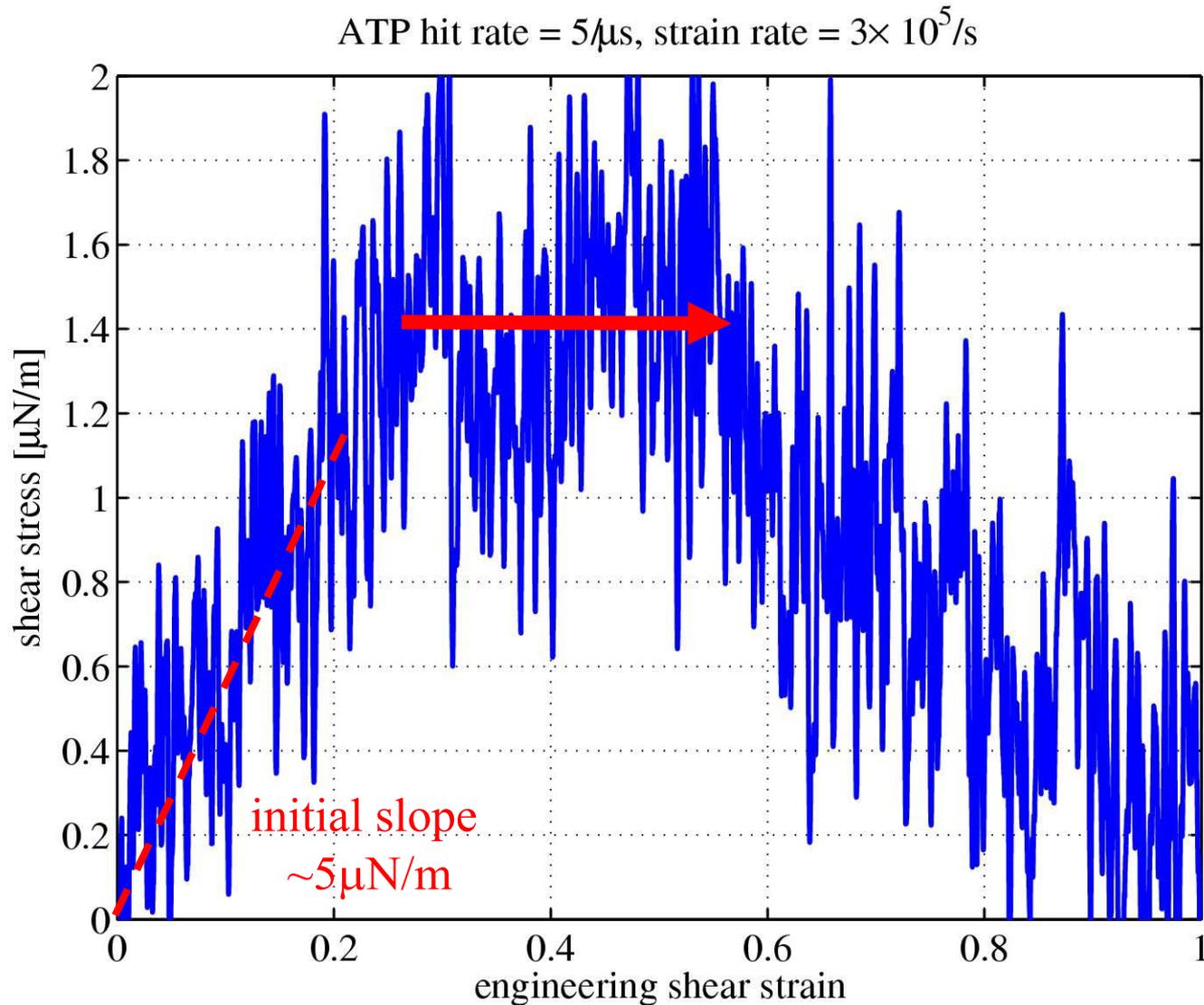


ATP hit rate =  $2/\mu\text{s}$ :  
two plastic displacements... also longer

ATP hit rate =  $2/\mu\text{s}$ , strain rate =  $3 \times 10^5/\text{s}$



# ATP hit rate = $5/\mu\text{s}$ : large-strain resistance collapses, manifest global yield



# Schematic Model of the RBC Membrane

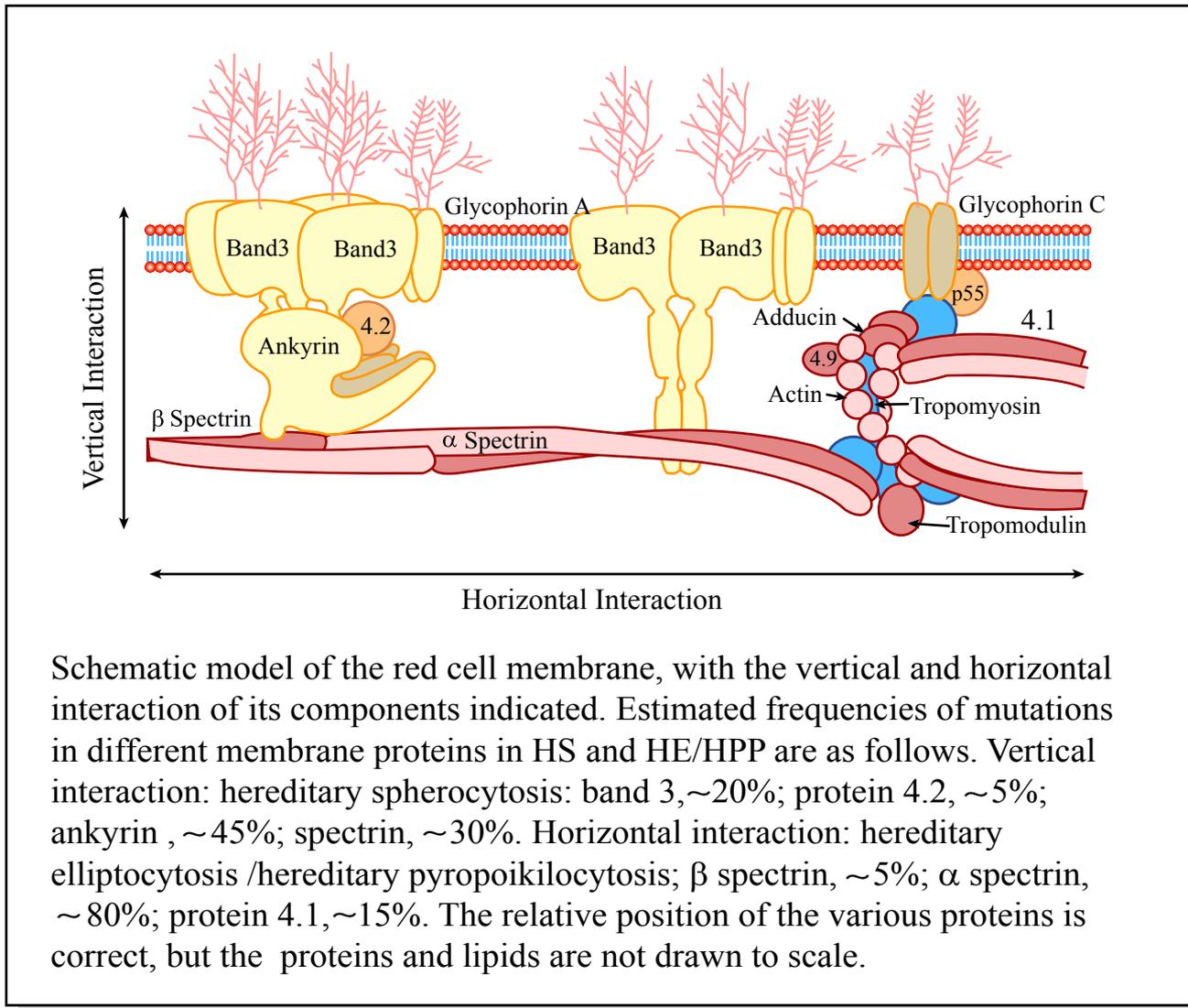


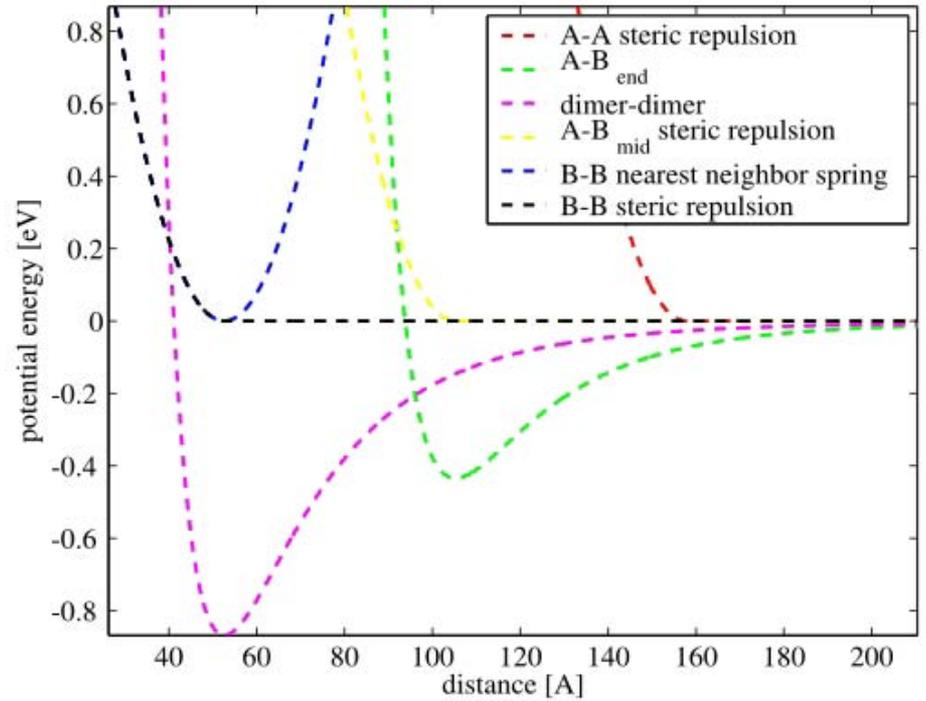
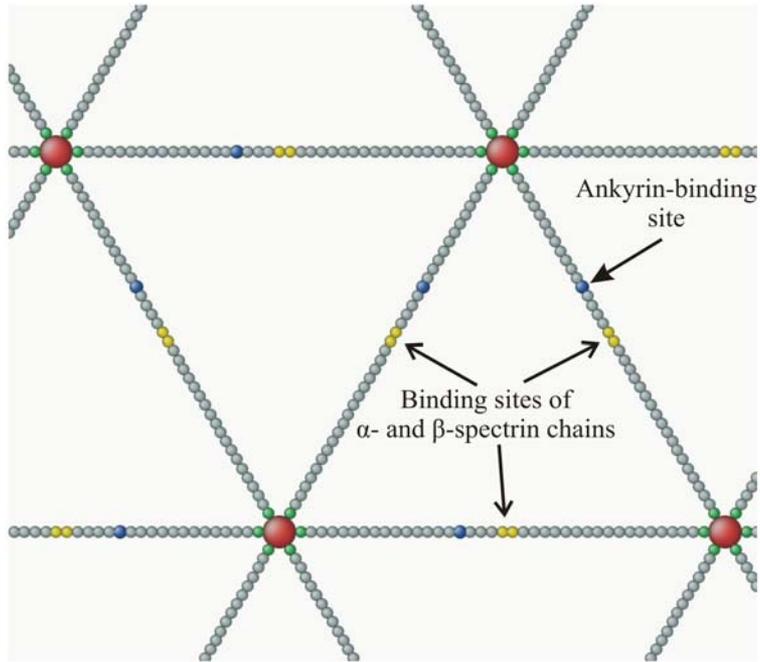
Figure by MIT OCW. After Tse and Lux, 1999.

Images removed due to copyright restrictions.

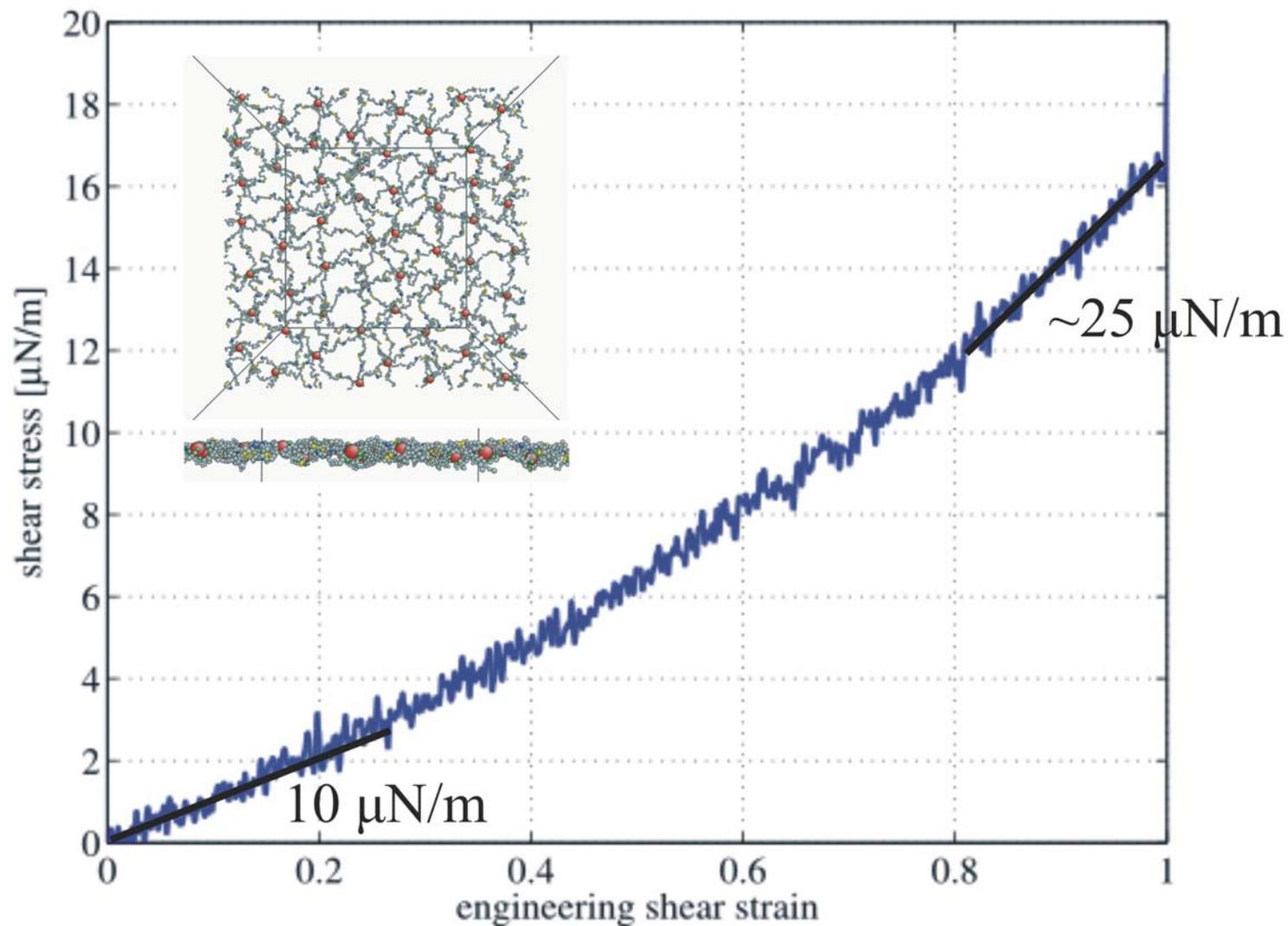
See figures in Discher, D. E., N. Mohandas, and E. A. Evans.

"Molecular Maps of Red Cell Deformations: Hidden Elasticity and in Situ Connectivity." *Science* 266 (1994): 1032-1038.

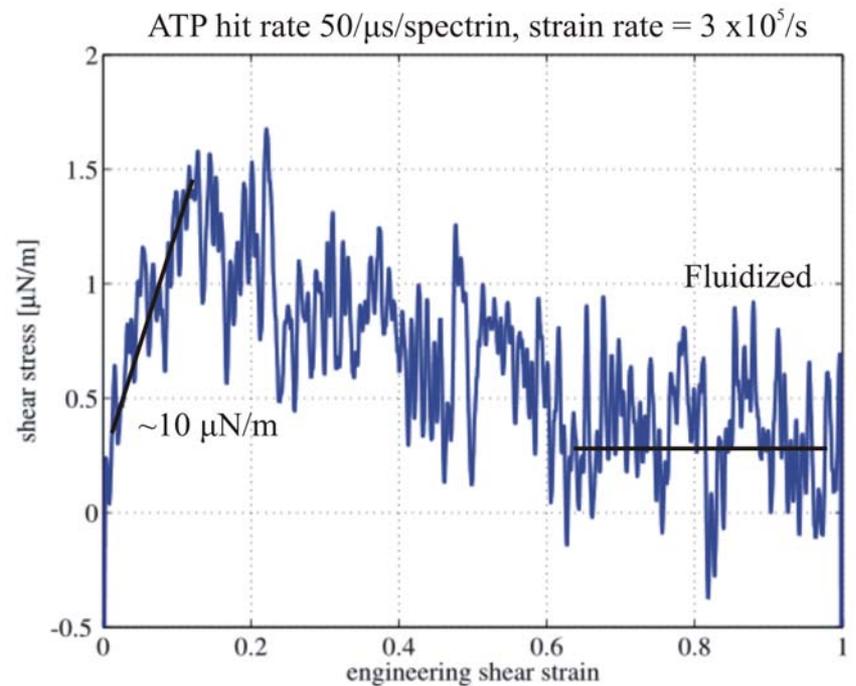
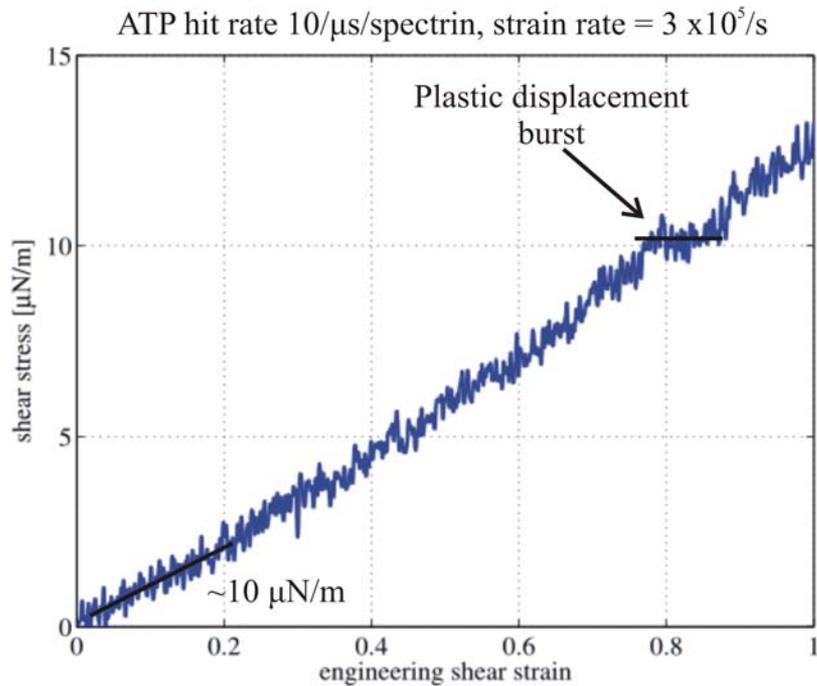
# Coarse Grain Molecular Dynamic Modeling



## Shear Deformation



## Shear Deformation and Promoted Dimer – Dimer Dissociation



# Summary

- A minimal CGMD model with *breakable* actin-spectrin junction has been developed, with physically reasonable parameters and behavior.
- ATP hydrolysis is modeled as stochastic kinetic energy transfer. As ATP hit rate rises, we see initiation of plastic displacement excursions, followed by macroscopic yield, and eventually, complete fluidization.
- Practical timescale of CGMD able to simulate recovery.